

Importance of Chewing Simulators in the Difference of Test Results of Dental Materials. Systematic Review

Abstract

Objectives:

With new dental materials constantly being launched on the market, the number of researches on the properties of dental materials have increased substantially in the past few years. However different results about physical properties of the same material are frequently found in the literature. In an endeavor to elucidate the cause(s) of these disparate results, a review of the literature published in the last five years was conducted, to investigate whether these differences are due to the testing machines - also called chewing simulators – used in the studies.

Data:

We searched for data of indicators of test accuracy, maintenance of test parameters during all experiments, reproducibility of test and standards in the articles, or in the manufacturers' sites.

Sources:

The database searched was CAPES PORTAL (<http://www-periodicos-capes-gov-br.ez27.periodicos.capes.gov.br>)

Study Selection:

In the search, the following keywords were used: "bite force" AND "simulator", "chewing simulator" and "mastication simulator", and the publication filter date of "January 1, 2016". As a result, 100 articles were selected and recovered in order of appearance by using the filter "relevance".

Conclusion:

based on the data obtained in this review, the disparate results of experiments with dental materials appeared to be more related to the test conditions rather than with the testing machines.

Keywords: Testing machines, chewing simulators, dental material, pre-clinical tests, systematic review.

1. Introduction

Since the end of the 19th century, there has been concern in dentistry about the progress of science and new technologies for improvement in clinical practice [1]. The number of materials and manufacturing methodologies have increased considerably in recent years. Knowledge of human bite force and the physical properties of restorative materials and their biocompatibility is fundamental in the practice of dentistry, in order to perform the required anatomical and functional restorations of the stomatognathic system (SS).

In the 19th century, Black [2] measured the bite force to understand the characteristics of the human tooth in relation to the pathologies that affected it and to obtain information in order to establish the physical properties necessary for a restorative material.

Correct chewing with an ideal bite force is a most important factor in the morpho-functional maintenance of the SS and brain health (brain-stomatognathic axis), since chewing stimulates the release of neurotransmitters such as serotonin, dopamine and mineralocorticoids in the central nervous system (CNS). These neurotransmitters contribute to well-being, protect against autonomic cardiac arrhythmias, improve the learning condition and slow brain aging [3,4,5,6,7,8,9,10]. Clearly, inadequate restorative procedures and/or materials can compromise these benefits provided by mastication.

Before testing a material in the mouth, it has to undergo a preclinical test to find out its resistance to fatigue, wear/aging, fracture and effect on antagonist teeth, among other properties. This is why the application of specific loads to this material is necessary to simulate the conditions of the SS by means of a testing machine. Another use of testing machines is to study the effects of chewing on food bolus [11,12]. There are simulators that serve both purposes, such as those made by SD Mechatronik (Mechatronik GMBH, Feldkirchen-Westerham) [13].

Due to the insertion of the CAD/CAM process of obtaining restorations and implants in dentistry, and the increasing numbers of polymers that can be used in this process, testing machines are fundamental, although they are not always used [14].

According to Heintze [14] some restorative materials have been for sale on the market for a long time without having undergone pre-clinical tests, especially metal porcelains, thereby placing patients at risk. Furthermore, Yiamaz et al [15] reported that in the last century, none of the wear test machines used in dentistry were included in an international standard. In 2001, standards were established for testing the wear resistance of dental materials in two- and three-body wear machines in accordance with the International Organization for Standardization (ISO) technical specifications [15].

In 2006, Heintze [16] conducted a study similar to the present review, and at the time, reported that only the MTS simulators (MTS Corp., Minneapolis, MN, USA) were qualified for in vitro wear testing. According to the author, the force exerted by the actuator was controlled and regulated throughout the test only in the MTS simulators. The weak reproducibility of the tests would be the explanation for the great variation of results found at the time.

The load simulators are divided into three major groups: static load simulators, dynamic load simulators and mixed simulators that can generate static and dynamic loads. Dynamic load simulators provide more data such as tension, bend, durability, high cycle fatigue, low cycle fatigue, compression, creep, fatigue crack growth, fracture toughness [17] than static load simulators, however, they have a higher cost and are less accessible to research (fewer job places on the bench) [14].

In this database search, the first simulator found in the literature was conceived by Head [18], who used a dry skull to determine the force necessary for crushing food during human chewing, with the purpose of using the information for the development of restorative materials. He performed the test by placing the skull upside down, then he attached a bucket to its jaw by means of wires, and placed weights in it(the bucket) to find out what pressure was needed for crushing the food.

The aim of this article was to review the literature in the last 5 years in order to evaluate the characteristics of the simulators used in the literature, based on the technical data found in the respective websites and/or in the published studies of customized simulators, to find out about the state of the art of simulators, their accuracy during the tests and the reproducibility of the tests.

2. Methodology

A search was conducted in two data bases, both accessed on 27/06/2020. with the following keywords: "bite force" AND "simulator", "chewing simulator" and "mastication simulator". In PUBMED (<https://pubmed.ncbi.nlm.nih.gov/>), using the date of publication filter “5 years” , 204 articles were found; and in CAPES PORTAL (<http://www-periodicos-capes-gov-br.ez27.periodicos.capes.gov.br>), using the date of publication filter “January 1, 2016” , 403 articles were found. We opted to use the data from the CAPES PORTAL data base. Out of the 403 articles found in the search, 100 articles were selected and recovered in order of appearance, by using the search parameter filter "relevance".

Three articles were excluded due to the methodology applied. They used no testing machine, only Finite Element Method Analysis [19,20,21].

In the other 97 articles, two distinct groups of chewing simulators were found: those manufactured by industries and for sale (from now on, this type will be referred to as commercialized simulators) and those developed by universities, research centers, research groups (from now on, these will be referred to as customized simulators). In the former group the technical information and standards were searched on the manufacturer's website. In the customized group, technical information was searched in the paper itself, or in another paper if this type were cited.

2.1 Testing machines for food study

Among the 100 studies recovered, 4 of them [11,12,13, 22] used the chewing simulator to study substances released while the food bolus was being chewed. Mohammadi, Ehsani and Bakhoda [13] used a Cs simulator from SD Mechatronics that will be evaluated later when evaluating the simulators for the study of property of restorative materials.

Mennis-Henrique et al [11]; Tarrega et al [12] used the customized simulator developed by Salles et al [23]. This simulator consisted of an active cell, where the chewing process was performed, an electronic control box and a computer to monitor and adjust each parameter. The active cell, composed of a movable jaw and a fixed jaw; both jaws were ring-shaped cylinders fitted with molars made of polyetheretherketone (PEEK) cylinders, and a tongue, exerting a force 30 dekanewtons, a shear force of 35 dekanewtons at an angle with value corresponding to 1/8 of the tooth. Although we had no access to more technical information, the data described in the studies led us to

believe that it was an efficient simulator that would allow test reproducibility and accuracy.

Peyron et al [22] used the AM2 chewing simulator that was validated by Woda et al [24]. This simulator had two discs, one fixed, corresponding to the maxilla, and one mobile, corresponding to the mandible. The shape of the discs differed from human dental anatomy, but were similar to contact surfaces at work as in human chewing. According to the authors, the food bolus resulting from crushing in the simulator was statistically equal to the food bolus crushed by human chewing with regard to particle size.

2.2 Chewing simulators for testing physical properties of materials

2.2.1 Customized

The customized simulators were used in 11 of the articles recovered. The chewing simulator developed by the University of Zurich was used by Ender et al [25], Zhi, Bortoloto and Krejci [26] for fatigue testing. According to the authors, it generated a load of 49 N, and the frequency and numbers of repetitions could be adjusted. In addition, it allowed a thermal cycling process operating between 5 and 50 degrees Celsius, with precision, frequency and load monitoring and controlling devices or system reported, but no standard was reported.

Singhatanadgit, Junkaew, Singhatanadgid [27] developed a chewing simulator for in vitro measurement of unidirectional and bidirectional loads. Systems for monitoring and controlling the frequency, precision and load were reported, but no standard was reported.

Gundugollu et al [28] developed a wear simulator consisting of two aluminum discs, one fixed bottom, and one upper rotating at 10 RPM driven by a Johnson engine with a capacity of 5 kg. According to the authors, the contact geometry was representative of masticatory function. They did not report any electronic process monitoring and controlling devices of precision and load, and any standard.

Guo et al [29] used a customized simulator developed by the Fourth Military Medical University. They used spheres as antagonists to investigate the tribological response of dental crowns to cyclic loads. After heat treatment, the spheres made of

stainless steel were similar to the natural enamel. The authors describe mechanisms for monitoring and controlling the process (precision, frequency, and load) in order to maintain the same conditions during the test and its reproducibility. No standard was reported.

Zipprich et al [30] used the Frankfurt chewing simulator that was designed and built specifically to test implant connections. A two-dimensional load could be applied, simulating the chewing forces as far as possible. Two actuators driven by Lorenz's force were used for load generation at a 90 degree angle. The strength and time variables were adjustable. The force produced by the actuators could be generated in arbitrary directions between +90° and -90° in relation to the long axis of the implant and ranged from zero to 300 N. Actuators were controlled by an electronic amplifier, which in turn, were controlled by the labview graphics programming system® [31]. From the authors' description, this simulator was a machine that allowed the same conditions (precision, frequency and load) to be maintained throughout the test, and reproducibility of the test [30,31].

Dayan et al [32] used the chewing simulator developed by the University of Selcuk, Research Laboratory Centre, Konya, Turkey). The simulation chambers were filled with artificial saliva that was maintained at 37° C throughout the test period and the occlusal contacts occurred under simulated physiological conditions. The dynamic load was obtained with a pin-on-block design with 0.5 mm glides at a frequency of 1.2 Hz with a constant load of 50 N per 20,000 cycles. No standard was reported.

Tahir et al [33] presented a chewing simulator that was developed to aid the placement of implants. It had a robotic chewing system with 6 degrees of freedom, with hydraulic actuators that replicated the action of the jaw in order to replicate the forces occurring in normal chewing. The authors reported a control system to maintain constant hydraulic pressure in the actuators. Test accuracy was guaranteed because the kinematic structure was a redundant robot arm - SCARA (Selective Compliance Assembly Robot Arm). Industrial grade systems have also been developed to conduct monotonic and cyclic tests, which are predominately uniaxial compression and tensile testers. These systems have also been used for (ISO) 14801 standardization testing.

Ip et al [34] developed a bite force simulator composed of pistons supported by a customized impression of the individual's skull obtained by 3D printing. Muscle loads were generated by proportional pressure controllers (PPC5C; MAC Valves, Wixom,

MI), operated by LabVIEW software by means of an analog voltage controller (National Instruments, Austin, TX), those devices control experiment conditions which guarantee accuracy and reproducibility, but no standard was reported.

Yilmaz et al [35], Yiamaz et al [36] idealized and produced a biaxial mastication simulator that exerted a 50 N load on the vertical axis and horizontal slide of 0.7 mm when the simulator came into touch with the studied specimen. This was controlled by magnetic sensors, so that after (touching the specimen) the load returned to the beginning allowing the load to be exerted at the same point, and accurately reported the point of force application, however, the authors did not report any frequency controlling systems or devices, nor standards.

2.2.2 Commercialized Simulators (for sale)

Passia, Ghazal and Kern [37], Yagizi, Kern and Chaar [38] used a computer-controlled biaxial chewing simulator; and Swain et al [39] used a universal fatigue simulator; Al Akhali et al [40], Asahhaf et al [41], and Yagizi et al [42] used the artificial aging machine simulating 5 years of use; all these items of equipment were manufactured by Willytec (Feldkirchen-Westerham, Germany). Willytec was the previous name of SD Mechatroniks[43].

Preis et al [44], Nalman et al [45], Preis et al [46], Kammermeier et al [47], von Stein-Lausnitz et al [48], Rosentritt et al [49] used the chewing simulator manufactured by EGO (Regensburg, Germany) with Willytec technology. This simulator allowed thermal cycling, operating between 5° and 55° C and testing with vertical and horizontal movements.. Apart from stating the Willytec technology, there was no report on the manufacturer's website, about standards used for the manufacture of simulators, or of devices or monitoring and control systems [50].

SD Mechatronik chewing simulators (Mechatronik GMBH, Feldkirchen-Westerham, Germany) CS 4.2 have been indicated for determination of the resistance to composite wear, fracture resistance of crowns, bridges and implants, and simulation of bruxism for interocclusal plate testing. According to the manufacturer they have a high degree of reproducibility of results because they allow identical kinematic conditions in each species placed in the test chambers. Model CS 4.8 simulates various masticatory movements to test implants, bridges, crowns, composites and jaw models. It performs the complete masticatory cycle through linear motion along 2 axes. It simulates chewing

frequency up to 5 Hz, simulates bruxism for interocclusal plate testing, and can offer real-time wear analysis. The two models provide thermal cycling operating between 5 and 55 degrees Celsius [51] and were used by Choi et al [52]; Koutousis, Gadalla, Lundgren [53]; Ladetski et al [54]; Yoon et al [55]; Askar et al [56], Elsayed et al [57]; Heintze et al [14]; Im et al [58]; Vafaei et al [59]; D'Arcangelo et al [60]; Elshyab et al [61]; Garoushi, Vallittu, Lassila [62]; Irmak et al [63]; Kewekordes, Wille, Kern [64]; Lehmensiek et al [65]; Mohammadi, Ehsani, Bakhoda [13]; Nawafleh et al [66]; Roulet, Abdulhameed, Shen [67]; Santos et al [68]; Sarikaya, Hayran [69]; Qasim, El-Masoud, Laban [70]; Zierden et al [71]; Agustin-Panadero et al [72]; Atsü et al [73]; Lassila et al [74]; Baumgart et al [75]; Dayan, Muncu [76]; Elkabbany, Kern, Elkhadem [77]; Lutz et al [78]; Riedel et al [79]; Sorrentino et al [80]; Hsu et al [81]; Zildan et al [82].

Stawarczyk et al [83] reported the use of CS 4.10 but the model was not found on the site. These simulators were all produced with Willytec technology. According to the site the simulators comply with the following standards: ISO 14801 :2017, ISO 6872: 2019, ISO 10477: 2017 and ISO / TS 14569 [51].

Instron (INSTRON, Norwood, MA, USA) manufactures several universal simulators that have proved to be efficient in pre-clinical tests, each related to the type of material tested. Huang, Chen, Lin [84] used the E3000 model. Ladetski et al [54] used model 4411 for static load testing. Mahmood et al [85] the Instron 4465, Pinto et al [86] the Instron 8501, Choi et al [87] used model 8871, Pedrollo Lise et al [88] used Instron 5848 MicroTester that tested laminates and bonding force. Allamari et al [89] reported the use of the universal test machine, capable of performing rupture tests at high temperatures, while Clausson et al [90] used the EMIC DL 2000 for determining the strength of materials in the following types of tests: tensile, compression, bending, bending, shear, pullout, delamination, adhesion, inlay, etc.; that is to say, all classes of destructive mechanical testing. This equipment, which performs rupture tests at high temperatures, is supplied with the Bluehill testing software. Sagsoz and Sagsoz [91] used the Instron/EMIC 3344 for fracture testing. Instron test machines comply with ISO 6892-2, EN 10002-5, ASTM E21 standards. [92]

Zwick/Roell (Ulm, Germany) offers several dynamic simulators, among which the choice depends on the properties of the material to be tested and the desired load. All models listed below were used for preclinical testing. According to the manufacturer all models have test control II, software that allows a very precise positioning of the tested part, measurement and test reproducibility. The Z050 model is indicated for

testing fatigue, indentation hardness and compression stress. All tests are performed in 3 phases: in the first, the thickness and hardness of indentation is measured, in the second, a fatigue load between 8.00 and 150,000 cycles is given, depending on the material tested and the next stage tests the reduction in thickness and the load for loss of interdentation; The Z 005 model offers compression testing up to 5 kN, and thermal testing; Model Z 1445 offers pressure of up to 10 kN indicated for fracture testing in flexible polymers. The Z010 model offers pressure of up to 10 kN, ZwickiLine 2.5 kN offers pressure of up to 2.5 kN [17]. (Nazari et al [93]; Stawarczyk et al [94]; Habibzadeh et al [95]; Sieper, Wille and Kern [96]; Alkharrat et al [97]; Elsayed et al [98] Obermeier et al [99]; Bishit et al [100], Jagodin et al [101]; kelch et al [102]; Nouhl et al [103], von Stein-launsnitz [48]; angermair [104]; Bunner and özcan [105]; Ioannidis et al [106]; Winter et al [107]). Zwick/Roell manufacturing test machines comply with ISO 9001 and 14001 standards [17].

Fathy and Swain [108] used the Robota Company chewing simulator (Alexandria, Egypt) equipped with servo-oriented steering system motors for horizontal and vertical movements, adjustment of distance of movement, integrated with thermal cycling and adjustment of the level of the active tip for accurate positioning [109].

Mieda et al [110] used the ANSYS program for finite element method study and Shimadzu's AG-10kNXplus universal test machine (Kyoto, Japan) for static and dynamic load testing. The device has trapezium x processing software that ensures reproducibility in all tests regarding the intensity and vector of load application and complies with ISO 6892: 2016 (JIS Z 2241:2011) standards [111].

Sedrez-Porto et al [112] and Silva et al [113] tested the fatigue of direct intracoronal restorations using the Biocycle V2 pneumatic chewing simulator from Biopdi (São Carlos, Brazil). This equipment performs mechanical fatigue tests that closely simulate the tests of the conditions found in the human mouth, and improves the in vitro study research methods that simulate human mastication. Compression or impact tests can be performed with forces that can range between 0 and 200kgf. Because it is powered by compressed air, it can reach frequencies of up to 5 Hz, without losing efficiency and up to 10 Hz in specific cases. It also has a sliding system for tests that best simulate masticatory movement, such as bruxism tests. It is provided with Software for making adjustments, configurations, acquisition, analysis and reporting of mechanical tests and complies with the NBR ABNT, ISO, ASTM, and DIN standards [114]

For dynamic fatigue tests, Katonaa and Eckert [115] and Kim et al [116] successfully used dynamic MTS Bionix 858 (MTS Corp., Minneapolis, MN, USA). Zhang et al [117] used the MTS Land-mark 370.10 model. MTS test machines feature hydraulic Servo innovations, versatile flextest control, and application software that provides high accuracy and reproducibility in high fidelity static and dynamic testing, and different types of stress, compression and fatigue tests and comparisons. All comply with ASTM D3039 standards, ASTM D2344, ASTM D790, ASTM D3518, ASTM D5023, ASTM D5024, ASTM D5026, ASTM D5418, ASTM D5992, ASTM D6272, ASTM D7028, ASTM E21, ASTM E290, ASTM E517, ASTM E646, ASTM E8-E8M, ASTM E9, ISO 10113, ISO 10275, ISO 14125, ISO 6892-1, ISO 6892-2, ISO 7438, ISO 14129, ISO 527-4, ISO 527-5, ISO 6721-4, ISO 6721-12, EN 2561 , EN 2562, EN 2597, EN 2746, EN 6031[118].

Bankoğlu Güngör, Karakoca Nemli [119]; Bankoğlu Güngör et al [120]; Rajic et al [121]; Sagsoz, Polat Sagsoz [122]; Sen, Us [123]; Benli et al [124] used the Mastication Simulator MOD (Esetron Smart Robotechnologies, Ankara, Turkey) a dynamic simulator that had a user-friendly interface and allowed remote monitoring during testing that allowed adjustment of all test parameters, including temperature. This equipment can be used for mono or biaxial tests and allows reproducibility of the tests. It is ideal for testing the physical properties of restorative materials or the study of impact of any event on dentition. Esetron test machines comply with ISO 9,100 ISO 12,100 [125].

Kim et al [116] used ADL-Force 5 (Advanced Mechanical Technology Inc., Watertown, MA, USA) for static mechanical fatigue testing. Force 5 could replicate the loading and full amplitude of multi-axis motion associated with daily activities. Four servo-hydraulic actuators control the movement of the mobile base through an electric motor. According to the manufacturer the test machine complies with the following standards: ISO-14242-1, ASTM-WK451, ASTM-F1612-95, ISO/DIS-7206-4, ISO-14243-1, ISO-14243-3, ASTM- F1715-00, ASTM-F1800-04, ASTM-F1223-05, ASTM-F2423-05, ISO/DIS-12189, ISO/DIS-18192-1, and ASTM-F1717-04 [126].

He et al [127] used a model LRX and D'Addazio et al [128] a model LR30K from Lloyd Instruments Ltd.,(Fareham, England), which complies with the ASTM D790, ISO 178, BS 2782 standards for flexural polymer testing. According to the technical data this equipment provide high accuracy and reproducibility. For flexural testing, the machines can compensate for the deflection of the equipment [129].

3. Results

All the data presented and discussed here from now on was based on the information reported in the articles. It is important to bear in mind that the testing machines may have had the systems or devices we were looking for, but since their presence was not reported in the articles we will consider that they were absent.

In relation to chewing simulators for the research of chewing effect on the food bolus found in 4 studies, 1 of them used a commercial chewing simulator from SD Mechatroniks manufactured in compliance with standards and with control and monitoring devices [13]. In two studies, the same simulator was used [11,12] and did not report any monitoring and control devices or systems. In one of the studies, a chewing simulator was used, and although there was no report of devices or monitoring and control systems, the equipment was validated with regard to the grinding capacity of the food bolus [22, 24].

Relative to the customized simulators for research of the physical properties of materials, 11 studies were found, yet only one [33] reported standards for the simulator.

The data* about the customized simulators used by Ender et al [25] and Zhi et al [26] developed by the university of Zurich, were* first published in 1999 by Kerjci et al [130], we could not recover complete text, but in the abstract they reported that it was a computer controlled simulator, so we inferred that it had a system for monitoring and controlling the experiment.

All the customized simulators were able to produce the experimental conditions of the commercialized types. When we considered the control systems or devices to maintain the same conditions throughout the entire experiment, eight studies reported precision, frequency and load control system for the simulator [25,26,27,29,30,31,32,33,34]. Only one article did not report precision or load control systems [28], and two did not report frequency control [35,36]. Table 1.

Table 1 Information about accuracy and reproducibility of customized simulators reported on the articles

Reference	Precision control	Frequency control	Load control	Standard
[25]	Yes	Yes	Yes	No
[26]	Yes	Yes	Yes	No
[27]	Yes	Yes	Yes	No

[28]	No	Yes	No	No
[29]	Yes	Yes	Yes	No
[30]	Yes	Yes	Yes	No
[32]	Yes	Yes	Yes	No
[33]	Yes	Yes	Yes	ISO 14801
[34]	Yes	Yes	Yes	No
[35][36]	Yes	No	Yes	No

Among the 82 studies recovered that used chewing commercialized simulators to study the physical properties of materials, 4 used 2 distinct simulators for static and dynamic load [48,54, 91,116]

In the present review were found commercialized simulators manufactured by Willytec, Mechatroniks GmbH, Instron, MTS Corp, Robota Company, eGo Kältesysteme GmbH, Zwick/Roell, Shimadzu, Biopdi, Esetron Smart Robotechnologies, Loyd and ADL (Advanced Mechanical Technology).

The most frequently found types were those with Willytec technology (Willytec, SD Mechatroniks, eGo Kältesysteme). As regards manufacturers, SD Mechatroniks simulators were the type most used. Table 2.

Only two manufacturers (eGo Kältesysteme and Robota company) did not show any references on their respective sites, with regard to technical standards for construction of the simulators. Since eGo Kältesysteme used Willytech technology we assumed that the simulators would comply with technical standards.

Only the eGo Kältesysteme did not mention monitoring and controlling system that would guarantee reproducibility and accuracy of the tests, since they used Willytec technology, we assumed that the simulators would have monitoring and controlling systems.

Based on the data obtained in this review we believe the testing machines themselves are not responsible for the disparate results found in the literature about physical properties of materials used for restorative purposes. This finding is in accordance with study of Sen & Us [123], who indicated that in addition to the test machine, test conditions with the number of fatigue cycles, load applied, simulated bone level, superstructure design, load indenter specifications, hydrothermal aging and load application angle were factors that could influence test results; therefore, tests conditions are more likely to influence the results nowadays, than the testing machines.

Table 2 Information obtained on the websites of manufacturers

Manufacturer as reported	Number of articles	Controlling systems	Technical standards
Willytec	6	Yes	Yes**
Mechatroniks GmbH	33	Yes	ISO 14801: 2017, 6872: 2019, 10477: 2017 & ISO / TS 14569
Instron	9	Yes	ISO 6892-2, EN 10002-5, ASTM E21
MTS Corp	3	Yes	ASTM D3039, D2344, D790, D3518, D5023, D5024, D5026, D5418, D5992, D6272, D7028, E21, E290, E517, E646, E8-E8M, E9, ISO 10113, 10275, 14125, 6892-1, 6892-2, 7438, 14129, 527-4, 527-5, 6721-4, 6721-12, EN 2561, 2562, 2597, 2746, 6031
eGo Kältersysteme GmbH	6	Yes**	Yes**
Lloyd Instruments Ltd	2	Yes	ASTM D790, ISO 178, BS 2782
Advanced Mechanical Technology Inc	1	Yes	ISO- 14242-1, ASTM-WK451, F1612-95, ISO/DIS- 7206-4, 18192-1, ISO-14243-1, 14243-3, ASTM- F1715-00, F1800-04, F1223-05, F2423-05, ISO/DIS- 12189, F1717-04
Esetron Smart Robotechnologies	4	Yes	ISO 9.100 ISO 12.100
Shimadzu	1	Yes	ISO 6892:2016 (JIS Z 2241:2011)
Biopdi	2	Yes	NBR ABNT, ISO, ASTM, DIN*
Robota Company	1	Yes	No
Zwick/Roell	16	Yes	ISO 9001 & 14001

* no report of standard number

** since Willytec and Mechatroniks technology are the same test machine, and Ego Kältersysteme uses Willytec technology, although no information about the monitoring system was found on the website, they will be treated as the Mechatroniks simulator, with regard to these items.

When taking into consideration the ISO standards (<https://www.iso.org/home.html>), ASTM standards (<https://www.astm.org/>), European standards (<https://www.en-standard.eu/>), British standards (<https://www.bsigroup.com/en-GB/>) and Japanese Standards (<https://webdesk.jsa.or.jp/>) used by the test machine manufacturers, it was clear that the testing machines were capable of performing the

tests required for dental materials. The standards comprised 23 different physical tests, with 17 different types of materials

Conclusion

Based on the simulators studied in this review, it could be concluded that:

- The testing machines used for the study of food properties, reported systems for controlling and monitoring the experiment
- The majority of the customized testing machine appeared to be able to maintain and reproduce the experimental conditions throughout the experimental period.
- The commercialized test machines found in this review had systems that guaranteed the accuracy and reproducibility of the experiments
- Almost all commercialized test machine manufacturers (except one) in this review showed standards on the website, which guaranteed the accuracy and reproducibility of the experiments.
- Based on the data acquired in this study, it would appear that differences in test results of physical properties of materials could be more related to the parameters established for the test than to the accuracy and reproducibility of the test machines, or the correct choice of the test machine for the investigation.

REFERENCES

1. LAMB M. A.; Monthly Bibliography Of Dental Literature. The Dental Cosmos, 1895; XXXVII (5): 466-468.
2. BLACK G.V.. An Investigation Of The Physical Characters Of The Human Teeth In Relation To Their Diseases, And To Practical Dental operations Together With The Physical Characters Of Filling Materials. The Dental Cosmos, 1895 XXXVII (5): 469- 484.
3. AHLGREN J.. Mechanism of Mastication. Acta Odont. Scand., 1966, 24 (Suppl 44): 1-109.
4. AHLGREN J.; OWALL B.. Muscular Activity and Chewing Force: A Polygraphic Study of Human Mandibular Movements. Archs Oral Biol., 1970, 15, 271-280.
5. Koizumi S, Minamisawa S, Sasaguri K, Onozuka M, Sato S, Ono Y. Chewing reduces sympathetic nervous response to stress and prevents poststress arrhythmias in rats. Am J Physiol Heart Circ Physiol 301: H1551–H1558, 2011.
6. Miyake S, Yoshikawa G, Yamada K, Sasaguri KI, Yamamoto T, Onozuka M, et al. Chewing ameliorates stress-induced suppression of spatial memory by increasing glucocorticoid receptor expression in the hippocampus. Brain Res 2012;1446:34–9. <https://doi.org/10.1016/j.brainres.2012.01.011>.

7. Ohkubo C, Morokuma M, Yoneyama Y, Matsuda R, Lee JS. Interactions between occlusion and human brain function activities. *J Oral Rehabil* 2013;40:119–29. <https://doi.org/10.1111/j.1365-2842.2012.02316.x>.
8. Fukushima-Nakayama Y, Ono T, Ono T, Hayashi M, Inoue M, Wake H, et al. Reduced Mastication Impairs Memory Function. *J Dent Res* 2017;96:1058–66. <https://doi.org/10.1177/0022034517708771>.
9. Jou YT. Dental deafferentation and brain damage: A review and a hypothesis. *Kaohsiung J Med Sci* 2018;34:231–7. <https://doi.org/10.1016/j.kjms.2018.01.013>.
10. Saruta J, To M, Sakaguchi W, Kondo Y, Tsukinoki K. Brain-derived neurotrophic factor is reported to stress and chewing in saliva and salivary glands. *Jpn Dent Sci Rev* 2020;56:43–9. <https://doi.org/10.1016/j.jdsr.2019.11.001>.
11. Menis-Henrique MEC, Janzantti NS, Andriot I, Sémon E, Berdeaux O, Schlich P, et al. Cheese-flavored expanded snacks with low lipid content: Oil effects on the in vitro release of butyric acid and on the duration of the dominant sensations of the products. *Lwt* 2019;105:30–6. <https://doi.org/10.1016/j.lwt.2019.01.052>.
12. Tarrega A, Yven C, Semon E, Mielle P, Salles C. Effect of oral physiology parameters on in-mouth aroma compound release using lipoprotein matrices: An in vitro approach. *Foods* 2019;8. <https://doi.org/10.3390/foods8030106>.
13. Mohammadi N, Ehsani MR, Bakhoda H. Design and Evaluation of the Release Characteristics of Caffeine-Loaded Microcapsules in a Medicated Chewing Gum Formulation. *Food Biophys* 2018;13:240–9. <https://doi.org/10.1007/s11483-018-9530-y>.
14. Heintze SD, Eser A, Monreal D, Rousson V. Using a chewing simulator for fatigue testing of metal ceramic crowns. *J Mech Behav Biomed Mater* 2017;65:770–80. <https://doi.org/10.1016/j.jmbbm.2016.09.002>.
15. Yilmaz E, Sadeler R, Duymuş Z, Özdoğan A. Effect of ambient pH and different chewing cycle of contact wear on dental composite material. *Dent Med Res* 2018;6:46. https://doi.org/10.4103/dmr.dmr_26_18.
16. Heintze SD. How to qualify and validate wear simulation devices and methods. *Dent Mater* 2006;22:712–34. <https://doi.org/10.1016/j.dental.2006.02.002>.
17. <https://www.zwickroell.com>. Acesso 07/06/2020
18. Head J. The Human Skull Used as A Gnathodynamometer To Determine The Value of Trituration in the Mastication of Food. *The Dental Cosmos* 1906; XVIII; 12, 1189-1192.
19. Hussein FA, Salloomi KN, Abdulrahman BY, Al-Zahawi AR, Sabri LA. Effect of thread depth and implant shape on stress distribution in anterior and posterior regions of mandible bone: A finite element analysis. *Dent Res J (Isfahan)* 2019;16:200–7. <https://doi.org/10.4103/1735-3327.255745>.
20. Prados-Privado M, Gehrke SA, Rojo R, Prados-Frutos JC. Complete mechanical characterization of an external hexagonal implant connection: in vitro study, 3D FEM, and probabilistic fatigue. *Med Biol Eng Comput* 2018;56:2233–44. <https://doi.org/10.1007/s11517-018-1846-8>.

21. Skamniotis CG, Elliott M, Charalambides MN. On modelling the constitutive and damage behaviour of highly non-linear bio-composites - Mesh sensitivity of the viscoplastic-damage law computations. *Int J Plast* 2019;114:40–62. <https://doi.org/10.1016/j.ijplas.2018.10.001>.
22. Peyron MA, Santé-Lhoutellier V, Dardevet D, Hennequin M, Rémond D, François O, et al. Addressing various challenges related to food bolus and nutrition with the AM2 mastication simulator. *Food Hydrocoll* 2019;97:105229. <https://doi.org/10.1016/j.foodhyd.2019.105229>.
23. Salles C, Tarrega A, Mielle P, Maratray J, Gorria P, Liaboeuf J, et al. Development of a chewing simulator for food breakdown and the analysis of in vitro flavor compound release in a mouth environment. *J Food Eng* 2007;82:189–98. <https://doi.org/10.1016/j.jfoodeng.2007.02.008>.
24. Woda A, Mishellany-Dutour A, Batier L, François O, Meunier JP, Reynaud B, et al. Development and validation of a mastication simulator. *J Biomech* 2010;43:1667–73. <https://doi.org/10.1016/j.jbiomech.2010.03.002>.
25. Ender A, Bienz S, Mörmann W, Mehl A, Attin T, Stawarczyk B. Marginal adaptation, fracture load and macroscopic failure mode of adhesively luted PMMA-based CAD/CAM inlays. *Dent Mater* 2016;32:e22–9. <https://doi.org/10.1016/j.dental.2015.11.009>.
26. Zhi L, Bortolotto T, Krejci I. Comparative in vitro wear resistance of CAD/CAM composite resin and ceramic materials. *J Prosthet Dent* 2016;115:199–202. <https://doi.org/10.1016/j.prosdent.2015.07.011>.
27. Singhatanadgit W, Junkaew P, Singhatanadgid P. Effect of bidirectional loading on contact and force characteristics under a newly developed masticatory simulator with a Dual-Direction loading system. *Dent Mater J* 2016;35:952–61. <https://doi.org/10.4012/dmj.2016-198>.
28. Gundugollu Y.; Yalavarthy R.; Krishna M.; Kalluri S.; Pydi S.; Tedlapu S. Comparison of the effect of monolithic and layered zirconia on natural teeth wear: An in vitro study. *The Journal of Indian Prosthodontic Society* 2018; 18(4): 336-342
29. Guo J, Li D, Wang H, Yang Y, Wang L, Guan D, et al. Effect of contact stress on the cycle-dependent wear behavior of ceramic restoration. *J Mech Behav Biomed Mater* 2017;68:16–25. <https://doi.org/10.1016/j.jmbbm.2017.01.027>.
30. Zipprich H, Miatke S, Hmaidouch R, Lauer H-C. A New Experimental Design for Bacterial Microleakage Investigation at the Implant-Abutment Interface: An In Vitro Study. *Int J Oral Maxillofac Implants* 2016;31:37–44. <https://doi.org/10.11607/jomi.3713>.
31. Zipprich H. Micro-movements and micro-pump effect of implant-abutment-connection 2010. Test-Report for Konus K3Pro Dental Implants. <https://www.argondentalusa.com/wp-content/uploads/2019/05/Micro-movements-and-micro-pump-effect-of-implant-abutment-connection-report.pdf>. 2010
32. Dayan C, Kiseri B, Gencel B, Kurt H, Tuncer N. Wear resistance and microhardness of various interim fixed prosthesis materials. *J Oral Sci* 2019;61:447–53. <https://doi.org/10.2334/josnusd.18-0323>.

33. Tahir AM, Jilich M, Trinh DC, Cannata G, Barberis F, Zoppi M. Architecture and design of a robotic mastication simulator for interactive load testing of dental implants and the mandible. *J Prosthet Dent* 2019;122:389.e1-389.e8. <https://doi.org/10.1016/j.prosdent.2019.06.023>.
34. Ip KC, You P, Moore CC, Ferreira LM. Bite Force Simulator: A Novel Technique to Simulate Craniofacial Strain In Vitro. *J Craniofac Surg*. 2020;31(3):838-842. doi:10.1097/SCS.0000000000006091.
35. Yilmaz E, Sadeler R, Duymus ZY, Öcal M. Effects of Two-body Wear on Microfill, Nanofill, and Nanohybrid Restorative Composites. *Biomed Biotechnol Res J* 2017;1:25-8. 10.4103/bbrj.bbrj_36_17
36. Yilmaz E, Sadeler R, Duymuş Z, Özdoğan A. Effect of ambient pH and different chewing cycle of contact wear on dental composite material. *Dent Med Res* 2018;6:46. https://doi.org/10.4103/dmr.dmr_26_18.
37. Passia N, Ghazal M, Kern M. Long-term retention behaviour of resin matrix attachment systems for overdentures. *J Mech Behav Biomed Mater* 2016;57:88–94. <https://doi.org/10.1016/j.jmbbm.2015.11.038>.
38. Yazigi C, Kern M, Chaar MS. Influence of various bonding techniques on the fracture strength of thin CAD/CAM-fabricated occlusal glass-ceramic veneers. *J Mech Behav Biomed Mater* 2017;75:504–11. <https://doi.org/10.1016/j.jmbbm.2017.08.016>.
39. Swain M V., Coldea A, Bilkhair A, Guess PC. Interpenetrating network ceramic-resin composite dental restorative materials. *Dent Mater* 2016;32:34–42. <https://doi.org/10.1016/j.dental.2015.09.009>.
40. Al-Akhali M, Chaar MS, Elsayed A, Samran A, Kern M. Fracture resistance of ceramic and polymer-based occlusal veneer restorations. *J Mech Behav Biomed Mater* 2017;74:245–50. <https://doi.org/10.1016/j.jmbbm.2017.06.013>.
41. Alsahhaf A, Spies BC, Vach K, Kohal RJ. Fracture resistance of zirconia-based implant abutments after artificial long-term aging. *J Mech Behav Biomed Mater* 2017;66:224–32. <https://doi.org/10.1016/j.jmbbm.2016.11.018>.
42. Yazigi C, Schneider H, Chaar MS, Rüger C, Haak R, Kern M. Effects of artificial aging and progression of cracks on thin occlusal veneers using SD-OCT. *J Mech Behav Biomed Mater* 2018;88:231–7. <https://doi.org/10.1016/j.jmbbm.2018.08.017>.
43. https://www.researchgate.net/publication/308179328_Using_a_chewing_simulator_for_fatigue_testing_of_metal_ceramic_crowns. Acess 09/07/2020
44. Preis V, Kammermeier A, Handel G, Rosentritt M. In vitro performance of two-piece zirconia implant systems for anterior application. *Dent Mater* 2016;32:765–74. <https://doi.org/10.1016/j.dental.2016.03.028>.
45. Naumann M, von Stein-Lausnitz M, Rosentritt M, Walter C, Meyer-Lückel H, Sterzenbach G. Impact of simulated reduced alveolar bone support, increased tooth mobility, and distal post-supported, root-treated abutment tooth on load capability of all-ceramic zirconia-supported cantilever FDP. *Clin Oral Investig* 2018;22:2799–807. <https://doi.org/10.1007/s00784-018-2366-5>.
46. Preis V, Hahnel S, Behr M, Rosentritt M. In vitro performance and fracture resistance of novel CAD/CAM ceramic molar crowns loaded on implants and

- human teeth. *J Adv Prosthodont* 2018;10:300–7.
<https://doi.org/10.4047/jap.2018.10.4.300>.
47. Kammermeier A, Rosentritt M, Behr M, Schneider-Feyrer S, Preis V. In vitro performance of one- and two-piece zirconia implant systems for anterior application. *J Dent* 2016;53:94–101. <https://doi.org/10.1016/j.jdent.2016.08.004>.
 48. von Stein-Lausnitz M, Bruhnke M, Rosentritt M, Sterzenbach G, Bitter K, Frankenberger R, et al. Direct restoration of endodontically treated maxillary central incisors: post or no post at all? *Clin Oral Investig* 2019;23:381–9. <https://doi.org/10.1007/s00784-018-2446-6>.
 49. Rosentritt M, Schumann F, Krifka S, Preis V. Influence of zirconia and lithium disilicate tooth-or implant-supported crowns on wear of antagonistic and adjacent teeth. *J Adv Prosthodont* 2020;12:1–8.
<https://doi.org/10.4047/jap.2020.12.1.1>.
 50. <https://ego-kaeltesysteme.de>
 51. <https://sd-mechatronik.de>
 52. Choi JW, Bae IH, Noh TH, Ju SW, Lee TK, Ahn JS, et al. Wear of primary teeth caused by opposed allceramic or stainless steel crowns. *J Adv Prosthodont* 2016;8:43–52. <https://doi.org/10.4047/jap.2016.8.1.43>.
 53. Koutouzis T, Gadalla H, Lundgren T. Bacterial Colonization of the Implant-Abutment Interface (IAI) of Dental Implants with a Sloped Marginal Design: An in-vitro Study. *Clin Implant Dent Relat Res* 2016;18:161–7.
<https://doi.org/10.1111/cid.12287>.
 54. Ladetzki K, Mateos-Palacios R, Pascual-Moscardó A, Selva-Otaolaurruchi EJ. Effect of retention design of artificial teeth and implant-supported titanium CAD-CAM structures on fracture resistance. *J Clin Exp Dent* 2016;8:e113–8.
<https://doi.org/10.4317/jced.52228>.
 55. Yoon KJ, Park YB, Choi H, Cho Y, Lee JH, Lee KW. Evaluation of stability of interface between CCM (Co-Cr-Mo) UCLA abutment and external hex implant. *J Adv Prosthodont* 2016;8:465–71. <https://doi.org/10.4047/jap.2016.8.6.465>.
 56. Askar H, Brouwer F, Lehmensiek M, Paris S, Schwendicke F. The association between loading of restorations and secondary caries lesions is moderated by the restoration material elasticity. *J Dent* 2017;58:74–9.
<https://doi.org/10.1016/j.jdent.2017.01.002>.
 57. Elsayed A, Meyer G, Wille S, Kern M. Influence of the yttrium content on the fracture strength of monolithic zirconia crowns after artificial aging. *Quintessence Int* 2019;50:344–8. <https://doi.org/10.3290/j.qi.a42097>.
 58. Im SM, Huh YH, Cho LR, Park CJ. Comparison of the fracture resistances of glass fiber mesh- and metal mesh-reinforced maxillary complete denture under dynamic fatigue loading. *J Adv Prosthodont* 2017;9:22–30.
<https://doi.org/10.4047/jap.2017.9.1.22>.
 59. Vafae F, Firouz F, Khoshhal M, Hooshyarfard A, Shahbazi A, Roshanaei G. Fatigue Fracture Strength of Implant-Supported Full Contour Zirconia and Metal Ceramic Fixed Partial Dentures. *J Dent (Tehran)* 2017;14:165–72.

60. D'Arcangelo C, Vanini L, Rondoni GD, Vadini M, De Angelis F. Wear evaluation of prosthetic materials opposing themselves. *Oper Dent* 2018;43:38–50. <https://doi.org/10.2341/16-212-L>.
61. Elshiyab SH, Nawafleh N, Walsh L, George R. Fracture resistance and survival of implant-supported, zirconia-based hybrid-abutment crowns: Influence of aging and crown structure. *J Investig Clin Dent* 2018;9:e12355. <https://doi.org/10.1111/jicd.12355>.
62. Garoushi S, Vallittu PK, Lassila L. Characterization of fluoride releasing restorative dental materials. *Dent Mater J* 2018;37:293–300. <https://doi.org/10.4012/dmj.2017-161>.
63. Irmak Ö, Yaman BC, Lee DY, Orhan EO, Mante FK, Ozer F. Flexural strength of fiber reinforced posts after mechanical aging by simulated chewing forces. *J Mech Behav Biomed Mater* 2018;77:135–9. <https://doi.org/10.1016/j.jmbbm.2017.09.001>.
64. Kewekordes T, Wille S, Kern M. Wear of polyetherketoneketones — Influence of titanium dioxide content and antagonistic material. *Dent Mater* 2018;34:560–7. <https://doi.org/10.1016/j.dental.2017.12.009>.
65. Lehmensiek M, Askar H, Brouwer F, Blunck U, Paris S, Schwendicke F. Restoration integrity, but not material or cementation strategy determined secondary caries lesions next to indirect restorations in vitro. *Dent Mater* 2018;34:e317–23. <https://doi.org/10.1016/j.dental.2018.09.004>.
66. Nawafleh N, Hatamleh MM, Öchsner A, Mack F. The Impact of Core/Veneer Thickness Ratio and Cyclic Loading on Fracture Resistance of Lithium Disilicate Crown. *J Prosthodont* 2018;27:75–82. <https://doi.org/10.1111/jopr.12473>.
67. Roulet JF, Abdulhameed N, Shen C. In vitro Wear of Three Bulk Fill Composites and Enamel. *Stomatology edu journal*, 01 December 2017, Vol.4(4), pp.248-253
68. Santos F, Branco A, Polido M, Serro AP, Figueiredo-Pina CG. Comparative study of the wear of the pair human teeth/Vita Enamic® vs commonly used dental ceramics through chewing simulation. *J Mech Behav Biomed Mater* 2018;88:251–60. <https://doi.org/10.1016/j.jmbbm.2018.08.029>.
69. Sarikaya I, Hayran Y. Effects of dynamic aging on the wear and fracture strength of monolithic zirconia restorations. *BMC Oral Health* 2018;18:1–7. <https://doi.org/10.1186/s12903-018-0618-z>.
70. Qasim TK, El-Masoud BM, Laban AMA. The effect of resistance grooves on the fracture toughness of zirconia-based crowns from mono and cyclic loading. *European Journal of Dentistry*, 2019, Vol.12(04), pp.491-495
71. Zierden K, Acar J, Rehmann P, Wöstmann B. Wear and Fracture Strength of New Ceramic Resins for Chairside Milling. *Int J Prosthodont* 2017;74–7. <https://doi.org/10.11607/ijp.5492>.
72. Agustín-Panadero R, Serra-Pastor B, Roig-Vanaclocha A, Fons-Font A, Solá-Ruiz MF. Fracture resistance and the mode of failure produced in metal-free crowns cemented onto zirconia abutments in dental implants. *PLoS One* 2019;14:1–12. <https://doi.org/10.1371/journal.pone.0220551>.

73. Atsü S, Aksan M, Bulut A. Fracture Resistance of Titanium, Zirconia, and Ceramic-Reinforced Polyetheretherketone Implant Abutments Supporting CAD/CAM Monolithic Lithium Disilicate Ceramic Crowns After Aging. *Int J Oral Maxillofac Implants* 2019;34:622–30. <https://doi.org/10.11607/jomi.7036>.
74. Lassila L, Säilynoja E, Prinssi R, Vallittu P, Garoushi S. Characterization of a new fiber-reinforced flowable composite. *Odontology* 2019;107:342–52. <https://doi.org/10.1007/s10266-018-0405-y>.
75. Baumgart P, Kirsten H, Haak R, Olms C. Biomechanical properties of polymer-infiltrated ceramic crowns on one-piece zirconia implants after long-term chewing simulation. *Int J Implant Dent* 2018;4:1–7. <https://doi.org/10.1186/s40729-018-0127-5>.
76. Dayan SÇ, Mumcu E. Effect of different storage media on the microhardness and wear resistance of resin-matrix ceramics. *Int J Appl Ceram Technol* 2019;16:2467–73. <https://doi.org/10.1111/ijac.13307>.
77. Elkabbany A, Kern M, Elkhadem AH, Wille S, A. Amer A, Chaar MS. Retention of metallic and non-metallic double-crown-retained mandibular overdentures on implants: An in-vitro study. *J Prosthodont Res* 2020:1–7. <https://doi.org/10.1016/j.jpor.2019.11.001>.
78. Lutz AM, Hampe R, Roos M, Lümke N, Eichberger M, Stawarczyk B. Fracture resistance and 2-body wear of 3-dimensional–printed occlusal devices. *J Prosthet Dent* 2019;121:166–72. <https://doi.org/10.1016/j.prosdent.2018.04.007>.
79. Riedel C, Wendler M, Belli R, Petschelt A, Lohbauer U. In vitro lifetime of zirconium dioxide-based crowns veneered using Rapid Layer Technology. *Eur J Oral Sci* 2019;127:179–86. <https://doi.org/10.1111/eos.12604>.
80. Sorrentino R, Navarra CO, Lenarda R Di, Breschi L, Zarone F, Cadenaro M, et al. Effects of finish line design and fatigue cyclic loading on phase transformation of zirconia dental ceramics: A qualitative micro-raman spectroscopic analysis. *Materials (Basel)* 2019;16. <https://doi.org/10.3390/ma12060863>.
81. Hsu PY, Ramos V, Sadr A. Microcomputed tomography evaluation of cement shrinkage under zirconia versus lithium disilicate veneers. *J Prosthet Dent* 2020:1–9. <https://doi.org/10.1016/j.prosdent.2020.01.021>.
82. Zidan S, Silikas N, Haider J, Alhotan A, Jahantigh J, Yates J. Evaluation of Equivalent Flexural Strength for Complete Removable Dentures Made of Zirconia-Impregnated PMMA Nanocomposites. *Materials (Basel)* 2020;13:2580. <https://doi.org/10.3390/ma13112580>.
83. Stawarczyk B, Frevert K, Ender A, Roos M, Sener B, Wimmer T. Comparison of four monolithic zirconia materials with conventional ones: Contrast ratio, grain size, four-point flexural strength and two-body wear. *J Mech Behav Biomed Mater* 2016;59:128–38. <https://doi.org/10.1016/j.jmbbm.2015.11.040>.
84. Huang SF, Chen WR, Lin CH. Biomechanical interactions of endodontically treated tooth implant-supported prosthesis under fatigue test with acoustic emission monitoring. *BioMed Eng OnLine*, vol 15, 23-33, 2016. <https://doi.org/10.4047/jap.2017.9.1.22>

85. Mahmood DJH, Linderoth EH, Wennerberg A, Von Steyern PV. Influence of core design, production technique, and material selection on fracture behavior of yttria-stabilized tetragonal zirconia polycrystal fixed dental prostheses produced using different multilayer techniques: Split-file, over-pressing, and manual. *Clin Cosmet Investig Dent* 2016;8:15–27. <https://doi.org/10.2147/CCIDE.S94343>.
86. Pinto PA, Colas G, Filleter T, De Souza GM. Surface and mechanical characterization of dental Yttria-Stabilized Tetragonal Zirconia Polycrystals (3Y-TZP) after different aging processes. *Microsc Microanal* 2016;22:1179–88. <https://doi.org/10.1017/S1431927616011843>.
87. Choi JW, Kim SY, Bae JH, Bae E Bin, Huh JB. In vitro study of the fracture resistance of monolithic lithium disilicate, monolithic zirconia, and lithium disilicate pressed on zirconia for three-unit fixed dental prostheses. *J Adv Prosthodont* 2017;9:244–51. <https://doi.org/10.4047/jap.2017.9.4.244>.
88. Pedrollo Lise D, Van Ende A, De Munck J, Umeda Suzuki TY, Cardoso Vieira LC, Van Meerbeek B. Biomechanical behavior of endodontically treated premolars using different preparation designs and CAD/CAM materials. *J Dent* 2017;59:54–61. <https://doi.org/10.1016/j.jdent.2017.02.007>.
89. Alammari MR, Abdelnabi MH, Swelem AA. Effect of total occlusal convergence on fit and fracture resistance of zirconia-reinforced lithium silicate crowns. *Clin Cosmet Investig Dent* 2019;11:1–8. <https://doi.org/10.2147/CCIDE.S193326>.
90. Clausson C, Schroeder CC, Goloni PV, Farias FAR, Passos L, Zanetti RV. Fracture Resistance of CAD/CAM Lithium Disilicate of Endodontically Treated Mandibular Damaged Molars Based on Different Preparation Designs. *Int J Biomater* 2019;2019. <https://doi.org/10.1155/2019/2475297>.
91. Sagsoz O, Polat Sagsoz N. Chemical degradation of dental CAD/CAM materials. *Biomed Mater Eng* 2019;30:419–26. <https://doi.org/10.3233/BME-191063>.
92. <https://www.instron.com.br/pt-br/?region=Brasil>. Acesso 07/06/2020
93. Nazari V, Ghodsi S, Alikhasi M, Sahebi M, Shamshiri AR. Fracture Strength of Three-Unit Implant Supported Fixed Partial Dentures with Excessive Crown Height Fabricated from Different Materials. *J Dent (Tehran)* 2016;13:400–6.
94. Stawarczyk B, Liebermann A, Eichberger M, Güth JF. Evaluation of mechanical and optical behavior of current esthetic dental restorative CAD/CAM composites. *J Mech Behav Biomed Mater* 2016;55:1–11. <https://doi.org/10.1016/j.jmbbm.2015.10.004>.
95. Habibzadeh S, Rajati HR, Hajmiragha H, Esmailzadeh S, Kharazifard M. Fracture resistances of zirconia, cast Ni-Cr, and fiber-glass composite posts under all-ceramic crowns in endodontically treated premolars. *J Adv Prosthodont* 2017;9:170–5. <https://doi.org/10.4047/jap.2017.9.3.170>.
96. Sieper K, Wille S, Kern M. Fracture strength of lithium disilicate crowns compared to polymer-infiltrated ceramic-network and zirconia reinforced lithium silicate crowns. *J Mech Behav Biomed Mater* 2017;74:342–8. <https://doi.org/10.1016/j.jmbbm.2017.06.025>.
97. Alkharrat AR, Schmitter M, Rues S, Rammelsberg P. and Tooth – Implant-Supported Fixed Dental Prostheses 2017:1663–73.

98. Elsayed A, Wille S, Al-Akhali M, Kern M. Effect of fatigue loading on the fracture strength and failure mode of lithium disilicate and zirconia implant abutments. *Clin Oral Implants Res* 2018;29:20–7. <https://doi.org/10.1111/clr.13034>.
99. Obermeier M, Ristow O, Erdelt K, Beuer F. Mechanical performance of cement- and screw-retained all-ceramic single crowns on dental implants. *Clin Oral Investig* 2018;22:981–91. <https://doi.org/10.1007/s00784-017-2178-z>.
100. Bishti S, Jäkel C, Kern M, Wolfart S. Influence of different preparation forms on the loading-bearing capacity of zirconia cantilever FDPs. A laboratory study. *J Prosthodont Res* 2019;63:347–53. <https://doi.org/10.1016/j.jpor.2018.10.010>.
101. Jagodin S, Sasse M, Freitag-Wolf S, Kern M. Influence of attachment design and material on the retention of resin-bonded attachments. *Clin Oral Investig* 2019;23:1217–23. <https://doi.org/10.1007/s00784-018-2544-5>.
102. Kelch M, Schulz J, Edelhoff D, Sener B, Stawarczyk B. Impact of different pretreatments and aging procedures on the flexural strength and phase structure of zirconia ceramics. *Dent Mater* 2019;35:1439–49. <https://doi.org/10.1016/j.dental.2019.07.020>.
103. Nouh I, Kern M, Sabet AE, Aboelfadl AK, Hamdy AM, Chaar MS. Mechanical behavior of posterior all-ceramic hybrid-abutment-crowns versus hybrid-abutments with separate crowns—A laboratory study. *Clin Oral Implants Res* 2019;30:90–8. <https://doi.org/10.1111/clr.13395>.
104. Angermair J, Nolte D, Linsenmann R, Kunzelmann KH. The influence of storage temperature on fracture behavior of cryopreserved teeth—An in vitro study. *Clin Exp Dent Res* 2020;373–80. <https://doi.org/10.1002/cre2.283>.
105. Brunner KC, Özcan M. Load bearing capacity and Weibull characteristics of inlay-retained resin-bonded fixed dental prosthesis made of all-ceramic, fiber-reinforced composite and metal-ceramic after cyclic loading. *J Mech Behav Biomed Mater* 2020;109. <https://doi.org/10.1016/j.jmbbm.2020.103855>.
106. Ioannidis A, Bomze D, Hämmerle CHF, Hüsler J, Birrer O, Mühlemann S. Load-bearing capacity of CAD/CAM 3D-printed zirconia, CAD/CAM milled zirconia, and heat-pressed lithium disilicate ultra-thin occlusal veneers on molars. *Dent Mater* 2020;36:e109–16. <https://doi.org/10.1016/j.dental.2020.01.016>.
107. Winter A, Schurig A, Rasche E, Rösner F, Kanus L, Schmitter M. The flexural strength of CAD/CAM polymer crowns and the effect of artificial ageing on the fracture resistance of CAD/CAM polymer and ceramic single crowns. *J Mater Sci Mater Med* 2020;31. <https://doi.org/10.1007/s10856-019-6347-2>.
108. Fathy SM, Swain M V. In-vitro wear of natural tooth surface opposed with zirconia reinforced lithium silicate glass ceramic after accelerated ageing. *Dent Mater* 2018;34:551–9. <https://doi.org/10.1016/j.dental.2017.12.010>.
109. https://cac716d7-9a2a-447d-89c8-ab8352b49981.filesusr.com/ugd/99b9cf_e251a98c09784e5d94fddc542b15174a.pdf). Acesso 07/06/2020

110. Mieda M, Atsuta I, Matsushita Y, Morita T, Ayukawa Y, Tsukiyama Y, et al. The effective design of zirconia coping on titanium base in dental implant superstructure. *Dent Mater J* 2018;37:237–43. <https://doi.org/10.4012/dmj.2017-022>.
111. <https://www.shimadzu.com/an/index.html>
112. Sedrez-Porto JA, Münchow EA, Valente LL, Cenci MS, Pereira-Cenci T. New material perspective for endocrown restorations: Effects on mechanical performance and fracture behavior. *Braz Oral Res* 2019;33:1–12. <https://doi.org/10.1590/1807-3107bor-2019.vol33.0012>.
113. Silva PFD, Oliveira LRS, Braga SSL, Signori C, Armstrong SR, Soares CJ, et al. Effect of selective carious tissue removal on biomechanical behavior of class II bulk-fill dental composite restorations. *Dent Mater* 2018;34:1289–98. <https://doi.org/10.1016/j.dental.2018.05.014>.
114. <https://biopdi.com.br/>
115. Katona TR, Eckert GJ. The mechanics of dental occlusion and disclusion. *Clin Biomech* 2017;50:84–91. <https://doi.org/10.1016/j.clinbiomech.2017.10.009>.
116. Kim WH, Song ES, Ju KW, Lim D, Han D, Jung T, et al. between Single- and Multi-Directional Cyclic Modes on a Dental Implant System. *Materials* 2020; 13, 1545; doi:10.3390/ma13071545.
117. Zhang Z, Guo J, Sun Y, Tian B, Zheng X, Zhou M, et al. Effects of crystal refining on wear behaviors and mechanical properties of lithium disilicate glass-ceramics. *J Mech Behav Biomed Mater* 2018;81:52–60. <https://doi.org/10.1016/j.jmbbm.2018.02.023>.
118. <https://www.mts.com>
119. Bankoğlu Güngör M, Karakoca Nemli S. Fracture resistance of CAD-CAM monolithic ceramic and veneered zirconia molar crowns after aging in a mastication simulator. *J Prosthet Dent* 2018;119:473–80. <https://doi.org/10.1016/j.prosdent.2017.05.003>.
120. Bankoğlu Güngör M, Karakoca Nemli S, Yılmaz H, Aydın C. Fracture resistance of different implant supported ceramic abutment/crown systems. *Eur Oral Res* 2019;53:80–7. <https://doi.org/10.26650/eor.20199657>.
121. Rajic VB, Malčić AI, Kütük ZB, Gurgan S, Krmek SJ, Miletic I. Compressive strength of new glass ionomer cement technology based restorative materials after thermocycling and cyclic loading. *Acta Stomatol Croat* 2019;53:318–25. <https://doi.org/10.15644/asc53/4/2>.
122. Sagsoz O, Polat Sagsoz N. Chemical degradation of dental CAD/CAM materials. *Biomed Mater Eng* 2019;30:419–26. <https://doi.org/10.3233/BME-191063>.
123. Sen N, Us YO. Fatigue survival and failure resistance of titanium versus zirconia implant abutments with various connection designs. *J Prosthet Dent* n.d.;122:315.e1-315.e7. <https://doi.org/10.1016/j.prosdent.2019.05.036>.
124. Benli M, Eker Gümüş B, Kahraman Y, Gökçen-Rohlig B, Evlioğlu G, Huck O, et al. Surface roughness and wear behavior of occlusal splint materials

- made of contemporary and high-performance polymers. *Odontology* 2020; 108:240–50. <https://doi.org/10.1007/s10266-019-00463-1>.
125. <http://esetron.com/portfolio/occlusal-loading-chewing-simulator>
 126. <https://amti.biz/select%20product%20PDFs/Simulator%20machines/ADL%20Force%205%20description%20and%20specs.pdf>
 127. He J, Garoushi S, Säilynoja E, Vallittu PK, Lassila L. The effect of adding a new monomer “Phene” on the polymerization shrinkage reduction of a dental resin composite. *Dent Mater* 2019;35:627–35. <https://doi.org/10.1016/j.dental.2019.02.006>.
 128. D’Addazio G, Santilli M, Rollo ML, Cardelli P, Rexhepi I, Murmura G. Fracture resistance of Zirconia-reinforced lithium silicate ceramic crowns cemented with conventional or adhesive systems: An in vitro study. *Materials (Basel)* 2020;13. <https://doi.org/10.3390/MA13092012>.
 129. https://www.ametektest.com/-/media/ametekttest/download_links/lloyd-instruments-materials-testing-catalogue-2020.pdf?la=en
 130. Krejci I, Reich T, Lutz F, Albertoni M. In-vitro-Testverfahren zur Evaluation Dentaler Restaurationssysteme. 1. Computergesteuerter Kausimulator [An in vitro test procedure for evaluating dental restoration systems. 1. A computer-controlled mastication simulator]. *Schweiz Monatsschr Zahnmed.* 1990;100(8):953-960.