

Combining citizen science and deep learning to amplify expertise in neuroimaging

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1 **Abstract**

2 Big Data promises to advance science through data-driven discovery. However, many standard lab protocols rely on manual
3 examination, which is not feasible for large-scale datasets. Meanwhile, automated approaches lack the accuracy of expert
4 examination. We propose to 1) start with expertly labelled data, 2) amplify labels through web applications that engage citizen
5 scientists, and 3) train machine learning on amplified labels, to emulate the experts. Demonstrating this, we developed a
6 system to quality control brain magnetic resonance images. Expert-labeled data were amplified by citizen scientists through
7 a simple web interface. A deep learning algorithm was then trained to predict data quality, based on citizen scientist labels.
8 Deep learning performed as well as specialized algorithms for quality control (AUC=0.99). Combining citizen science and
9 deep learning can generalize and scale expert decision making; this is particularly important in disciplines where specialized,
10 automated tools do not yet exist.

11 **Author Summary**

12 How do we scale procedures that currently depend on human expertise to large-scale datasets? This is a
13 fundamental challenge in this era of Big Data, not unique to any one discipline, but particularly pertinent to
14 computational neuroimaging. For example, when studying pediatric mental health using brain MRI scans,
15 researchers would need to visually check the quality of hundreds of brain images. Instead, we developed a
16 web application (<https://braindr.us>) for citizen scientists to perform quality control of this large dataset
17 by swiping right (to pass) or left (to fail) each image. We aggregated the ratings with a machine learning
18 model, and then trained a deep neural network to automatically predict image quality, such that it matched
19 expert ratings. In other words, combining citizen science with deep learning through an intuitive web
20 application enabled us to amplify and automate expertise. This procedure will be broadly applicable to

21 the growing demands of Big Data across the sciences. An interactive version of this article is at [http://](http://results.braindr.us)
22 results.braindr.us .

23 Introduction

24 Many research fields ranging from astronomy, to genomics, to neuroscience are entering an era of Big Data.
25 Large and complex datasets promise to address many scientific questions, but they also present a new set
26 of challenges. For example, over the last few years human neuroscience has evolved into a Big Data field.
27 In the past, individual groups would each collect their own samples of data from a relatively small group
28 of individuals. More recently, large data sets collected from many thousands of individuals are increasingly
29 more common. This transition has been facilitated through assembly of large aggregated datasets, con-
30 taining measurements from many individuals, and collected through consortium efforts such as the Human
31 Connectome Project (Glasser et al., 2016). These efforts, and the large datasets that they are assembling,
32 promise to enhance our understanding of the relationship between brain anatomy, brain activity and cog-
33 nition. The field is experiencing a paradigm shift (Fan, Han, & Liu, 2014), where our once established
34 scientific procedures are morphing as dictated by the new challenges posed by large datasets. We've seen
35 a shift from desktop computers to cyberinfrastructure (Van Horn & Toga, 2013), from small studies siloed
36 in individual labs to an explosion of data sharing initiatives (Ferguson, Nielson, Cragin, Bandrowski, &
37 Martone, 2014; Poldrack & Gorgolewski, 2014), from idiosyncratic data organization and analysis scripts
38 to standardized file structures and workflows (K. J. Gorgolewski et al., 2016, 2017), and an overall shift in
39 statistical thinking and computational methods (Fan et al., 2014) that can accommodate large datasets. But
40 one often overlooked aspect of our protocols in neuroimaging has not yet evolved to the needs of Big Data:
41 expert decision making.

42 Specifically, decisions made by scientists with expertise in neuroanatomy and MRI methods (i.e., neuroimag-
43 ing experts) through visual inspection of imaging data cannot be accurately scaled to large datasets. For
44 example, when inspecting an MRI image of the brain, there is extensive variation in neuroanatomy across
45 individuals, and variation in image acquisition and imaging artifacts; knowing which of these variations are
46 acceptable versus abnormal comes with years of training and experience. Specific research questions require
47 even more training and domain expertise in a particular method, such as tracing anatomical regions of

48 interest (ROIs), editing fascicle models from streamline tractography (Jordan, Amirbekian, Keshavan, &
49 Henry, 2017), evaluating cross-modality image alignment, and quality control of images at each stage of
50 image processing. On large datasets, especially longitudinal multisite consortium studies, these expert de-
51 cisions cannot be reliably replicated because the timeframe of these studies is long, individual experts get
52 fatigued, and training teams of experts is time consuming, difficult and costly. As datasets grow to hundreds
53 of thousands of brains it is no longer feasible to depend on manual interventions.

54 One solution to this problem is to train machines to emulate expert decisions. However, there are many cases
55 in which automated algorithms exist, but expert decision-making is still required for optimal results. For
56 example, a variety of image segmentation algorithms have been developed to replace manual ROI editing,
57 with Freesurfer (Fischl, 2012), FSL (Patenaude, Smith, Kennedy, & Jenkinson, 2011), ANTS (Avants et al.,
58 2011), and SPM (Ashburner & Friston, 2005) all offering automated segmentation tools for standard brain
59 structures. But these algorithms were developed on a specific type of image (T1-weighted) and on a specific
60 type of brain (those of healthy controls). Pathological brains, or those of children or the elderly may violate
61 the assumptions of these algorithms, and their outputs often still require manual expert editing. Similarly,
62 in tractography, a set of anatomical ROIs can be used to target or constrain streamlines to automatically
63 extract fascicles of interest (Catani & Thiebautdeschotten, 2008; Yeatman, Dougherty, Myall, Wandell, &
64 Feldman, 2012). But again, abnormal brain morphology resulting from pathology would still require expert
65 editing (Jordan, Keshavan, et al., 2017). The delineation of retinotopic maps in visual cortex is another
66 task that has been recently automated (Benson, Butt, Brainard, & Aguirre, 2014; Benson et al., 2012),
67 but these procedures are limited to only a few of the known retinotopic maps and substantial expertise is
68 still required to delineate the other known maps (Winawer & Witthoft, 2017; Wandell & Winawer, 2011).
69 Another fundamental step in brain image processing that still requires expert examination is quality control.
70 There are several automated methods to quantify image quality, based on MRI physics and the statistical
71 properties of images, and these methods have been collected under one umbrella in an algorithm called
72 MRIQC (Esteban et al., 2017). However, these methods are specific to T1-weighted images, and cannot
73 generalize to different image acquisition methods. To address all of these cases, and scale to new, unforeseen
74 challenges, we need a general-purpose framework that can train machines to emulate experts for any purpose,
75 allowing scientists to fully realize the potential of Big Data.

76 One general solution that is rapidly gaining traction is deep learning. Specifically, convolutional neural
77 networks (CNNs) have shown promise in a variety of biomedical image processing tasks. Modeled loosely
78 on the human visual system, CNNs can be trained for a variety of image classification and segmentation
79 tasks using the same architecture. For example, the U-Net ([Ronneberger, Fischer, & Brox, 2015](#)) which was
80 originally built for segmentation of neurons in electron microscope images, has also been adapted to segment
81 macular edema in optical coherence tomography images ([Lee, Tying, et al., 2017b](#)), to segment breast and
82 fibroglandular tissue ([Dalms et al., 2017](#)), and a 3D adaptation was developed to segment the Xenopus
83 kidney ([Çiçek, Abdulkadir, Lienkamp, Brox, & Ronneberger, 2016](#)). Transfer learning is another broadly
84 applicable deep learning technique, where a number of layers from pretrained network are retrained for a
85 different use case. This can drastically cut down the training time and labelled dataset size needed ([Ahmed,
86 Yu, Xu, Gong, & Xing, 2008; Pan & Yang, 2010](#)). For example, the same transfer learning approach was
87 used for brain MRI tissue segmentation (gray matter, white matter, and CSF) and for multiple sclerosis
88 lesion segmentation ([Van Oproek, Ikram, Vernooij, & De Bruijne, 2015](#)). Yet despite these advances in
89 deep learning, there is one major constraint to generalizing these methods to new imaging problems: a large
90 amount of labelled data is still required to train CNNs. Thus, even with the cutting-edge machine learning
91 methods available, researchers seeking to automate these processes are still confronted with the original
92 problem: how does a single expert create an annotated dataset that is large enough to train an algorithm
93 to automate their expertise through machine learning?

94 We propose that citizen scientists are a solution. Specifically, we hypothesize that citizen scientists can learn
95 from, and amplify expert decisions, to the extent where deep learning approaches become feasible. Rather
96 than labelling hundreds or thousands of training images, an expert can employ citizen scientists to help with
97 this task, and machine learning can identify which citizen scientists provide expert-quality data. As a proof
98 of concept, we apply this approach to brain MRI quality control (QC): a binary classification task where
99 images are labelled “pass” or “fail” based on image quality. QC is a paradigmatic example of the problem of
100 scaling expertise, because a large degree of subjectivity still remains in QC. Each researcher has their own
101 standards as to which images pass or fail on inspection, and this variability may have problematic effects on
102 downstream analyses, especially statistical inference. Effect size estimates may depend on the input data
103 to a statistical model. Varying QC criteria will add more uncertainty to these estimates, and might result in
104 replication failures. For example, in ([Ducharme et al., 2016a](#)), the authors found that QC had a significant
105 impact on their estimates of the trajectory of cortical thickness during development. They concluded that

106 post-processing QC (in the form of expert visual inspection) is crucial for such studies, especially due to
107 motion artifacts in younger children. While this was feasible in their study of 398 subjects, this would
108 not be possible for larger scale studies like the ABCD study, which aims to collect data on 10,000 subjects
109 longitudinally (Casey et al., 2018). It is therefore essential that we develop systems that can accurately
110 emulate expert decisions, and that these systems are made openly available for the scientific community.

111 To demonstrate how citizen science and deep learning can be combined to amplify expertise in neuroimaging,
112 we developed a citizen-science amplification and CNN procedure for the openly available Healthy Brain
113 Network dataset (HBN; (Alexander et al., 2017)). The HBN initiative aims to collect and publicly release
114 data on 10,000 children over the next 6 years to facilitate the study of brain development and mental
115 health through transdiagnostic research. The rich dataset includes MRI brain scans, EEG and eye tracking
116 recordings, extensive behavioral testing, genetic sampling, and voice and actigraphy recordings. In order
117 to understand the relationship between brain structure (based on MRI) and behavior (EEG, eye tracking,
118 voice, actigraphy, behavioral data), or the association between genetics and brain structure, researchers
119 require high quality MRI data.

120

121 In this study, we crowd-amplify image quality ratings and train a CNN on the first and second data releases
122 of the HBN (n=722), which can be used to infer data quality on future data releases. We also demonstrate
123 how choice of QC threshold is related to the effect size estimate on the established association between age
124 and brain tissue volumes during development (Lebel & Beaulieu, 2011). Finally, we show that our approach
125 of deep learning trained on a crowd-amplified dataset matches state-of-the-art software built specifically for
126 image QC (Esteban et al., 2017). We conclude that this novel method of crowd-amplification has broad
127 applicability across scientific domains where manual inspection by experts is still the gold-standard.

128 **Results**

129 **Overview**

130 Our primary goals were to 1) amplify a small, expertly labelled dataset through citizen science, 2) train
131 a model that optimally combines citizen scientist ratings to emulate an expert, 3) train a CNN on the
132 amplified labels, and 4) evaluate its performance on a validation dataset. Figure 1 shows an overview of
133 the procedure and provides a summary of our results. At the outset, a group of neuroimaging experts
134 created a gold-standard quality control dataset on a small subset of the data (n=200), through extensive
135 visual examination of the full 3D volumes of the data. In parallel, citizen scientists were asked to “pass” or
136 “fail” two-dimensional axial slices from the full dataset (n=722) through a web application called braindr
137 that could be accessed through a desktop, tablet or mobile phone (<https://braindr.us>). Amplified labels,
138 that range from 0 (fail) to 1 (pass), were generated from citizen scientist ratings. A receiver operating
139 characteristic (ROC) curve was generated for both the ratings averaged across citizen scientists and labels
140 generated by fitting a classifier that weights ratings more heavily for citizen scientists who more closely
141 matched the experts in the subset rated by both (gold-standard). Next, a neural network was trained to
142 predict the weighted labels. The AUC for the predicted labels on a left out dataset was 0.99.

143

144 **Aggregating Citizen Scientist Ratings to Emulate Expert Labels**

145 Citizen scientists who rated images through the braindr web application differed substantially in terms of
146 how well their ratings matched the experts’ ratings on the gold-standard subset: while some provided high-
147 quality ratings that agree with the experts most of the time, others displayed variable and unreliable ratings.
148 In order to capitalize on citizen scientists to amplify expert ratings to new data, a weighting of each citizen
149 scientist was learned based on a reliable match to expert agreement in slices from the gold-standard set.
150 We used the XGBoost algorithm (Chen & Guestrin, 2016a), an ensemble method that combines a set of
151 weak learners (decision trees) to fit the gold-standard labels based on a set of features. In our case, the
152 features were the average rating of the slice image from each citizen scientist (some images were viewed and
153 rated more than once, so image ratings could vary between 1=always “pass” and 0=always “fail”). We then
154 used the weights to combine the ratings of the citizen scientists and predict the left out test set. Figure 2A

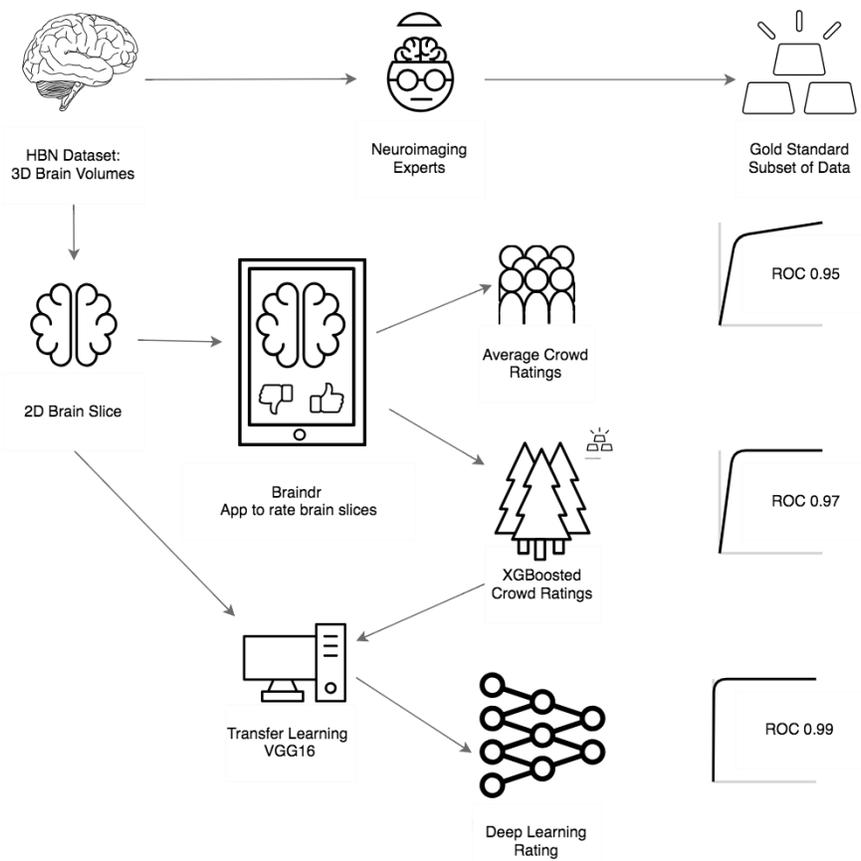


Figure 1: **Overview and results of our procedure:** First, the HBN data set was rated by 4 neuroimaging experts to create a gold standard subset of data. Next, the 3D MRI scans were converted into 2D axial brain slices, which were loaded onto braindr (<https://braindr.us>), a web application to crowdsource the quality ratings (see Methods). Area under the curve of a the Receiver Operating Characteristic curve (AUC) was calculated for the average citizen scientist quality rating for each slice. Compared to an expert-labeled test set, this resulted in an AUC of 0.95. In an effort to remove unreliable citizen scientists, the ratings were aggregated by fitting a model that weights each citizen scientist contribution to the slice score by how much that individual’s scores match those of the experts. The resulting AUC was 0.97. Finally, the 2D brain slices together with the weighted citizen scientist ratings were used to train a neural network. In an ROC analysis on left out data, the AUC of these predictions was 0.99.

155 shows ROC curves of classification on the left-out test set for different training set sizes, compared to the
 156 ROC curve of a baseline model in which equal weights were assigned to each citizen scientist. We see an
 157 improvement in the AUC of the XGBoosted labels (0.97) compared to the AUC of the equi-weighted labels
 158 (0.95). Using the model trained on two-thirds of the gold standard data (n=670 slices), we extracted the
 159 probability scores of the classifier on all slices (see Figure 2B). The distribution of probability scores in
 160 Figure 2B matches our expectations of the data; a bimodal distribution with peaks at 0 and 1, reflecting
 161 that images are mostly perceived as “passing” or “failing” . The XGBoost model also calculates a feature

162 importance score (F). F is the number of times that a feature (in our case, an individual citizen scientist)
 163 has split the branches of a tree, summed over all boosted trees. Figure 2C shows the feature importance for
 164 each citizen scientist, and 2D shows the relationship between a citizen scientist’s importance compared to
 165 the number of images they rated. In general, the more images a citizen scientist rates, the more important
 166 they are to the model. However, there are still exceptions where a citizen scientist rated many images and
 their ratings were incorrect or unreliable, so the model gave them less weight during aggregation.

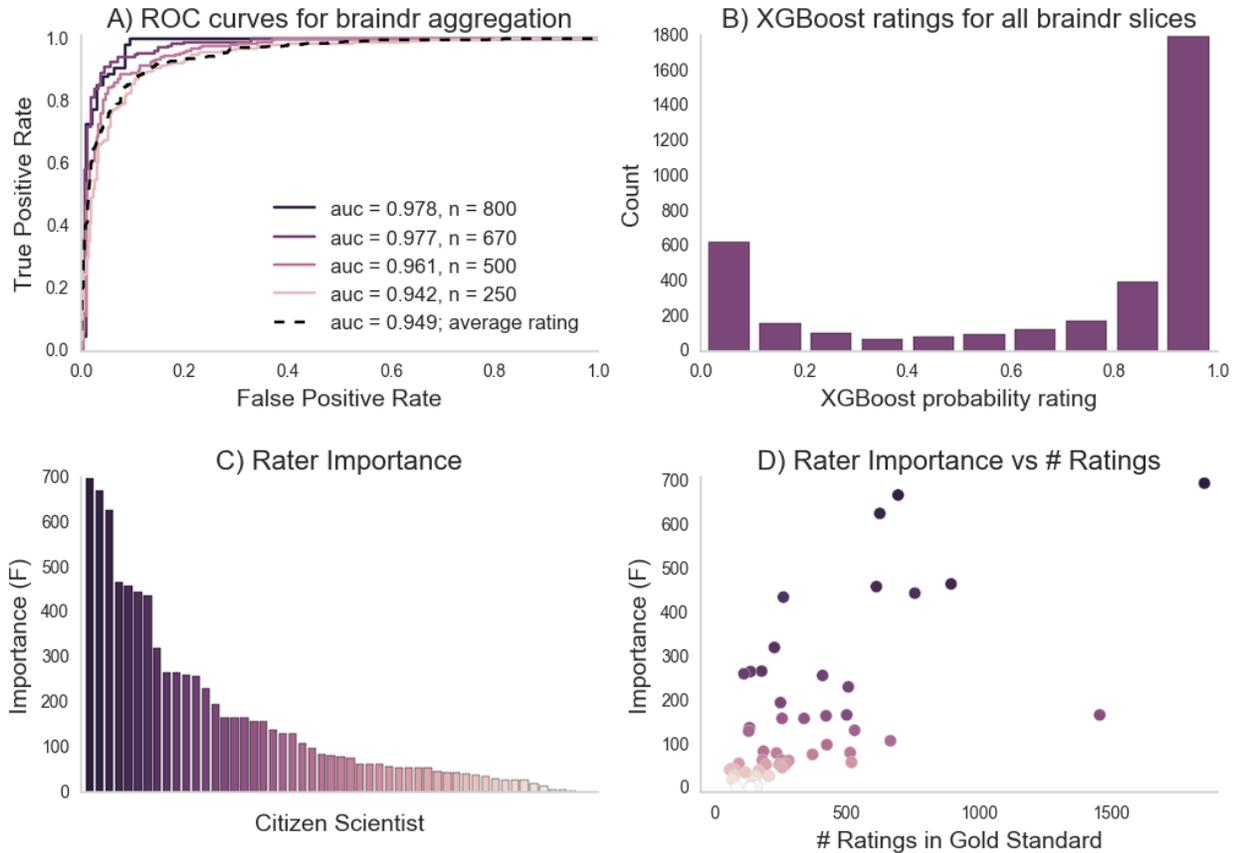


Figure 2: **Braindr rating aggregation and citizen scientist importance:** A. ROC curves on the test set for various training set sizes (here n denotes the number of training slices used). The dashed line is the ROC curve of the average citizen scientist ratings for all slices. B. The distribution of XGBoost probability scores on all Braindr slices. C. Feature importance for each anonymized user. D. Relationship between citizen scientist importance and total number of ratings in the gold-standard dataset.

167

168 Training Deep Learning to Automate Image Labeling

169 Citizen scientists accurately amplify expert ratings but, ideally, we would have a fully automated approach
 170 that can be applied to new data as it becomes available. Thus, we trained a deep learning model to

171 predict the XGBoosted labels that were based on aggregated citizen scientist ratings. A VGG16 neural
 172 network (Simonyan & Zisserman, 2014) pretrained on the ImageNet challenge dataset (Russakovsky et al.,
 173 2015) was used: we removed the top layer of the network, and then trained a final fully-connected layer
 174 followed by a single node output layer. The training of the final layer was run for 50 epochs and the best
 175 model on the validation set was saved. To estimate the variability of training, the model was separately
 176 trained through 10 different training courses, each time with a different random initialization seed. Typically,
 177 training and validation loss scores were equal at around 10 epochs, after which the model usually began to
 178 overfit (training error decreased, while validation error increased, see Figure 3A). In each of the 10 training
 179 courses, we used the model with the lowest validation error for inference on the held out test set, and
 180 calculated the ROC AUC. AUC may be a problematic statistic when the test-set is imbalanced (Saito &
 181 Rehmsmeier, 2015), but in this case, the test-set is almost perfectly balanced (see Methods). Thus, we
 182 found that a deep learning network trained on citizen scientist generated labels was a better match to expert
 183 ratings than citizen scientist generated labels alone: the deep learning model had an AUC of 0.99 (+/-
 standard deviation of 0.12, see Figure 3B).

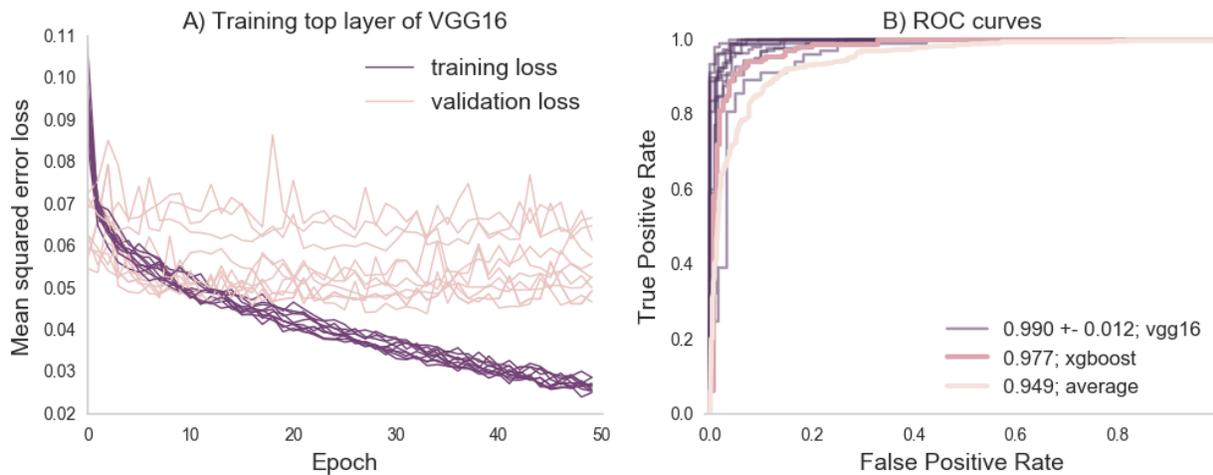


Figure 3: **Deep learning training and evaluation on the left out test set:** Part A shows the training and validation loss scores for 10 training runs, each with a different initialization seed. The training loss tends towards 0 but the validation loss plateaus between 0.05 and 0.07 mean squared error at the 10th epoch. Part B shows the ROC curve of the prediction on the test set against the binary classified gold-standard slices, along with the ROC curves computed from previous analysis (the average citizen scientist rating, and the XGBoosted ratings).

184

185 **Crowd amplification and deep learning strategy performs as well as a specialized** 186 **QC algorithm**

187 We validated our generalized approach of crowd-amplification and deep learning by comparing classification
188 results against an existing, specialized algorithm for QC of T1 weighted images, called MRIQC ([Esteban et](#)
189 [al., 2017](#)). The features extracted by MRIQC are guided by the physics of MR image acquisition and by the
190 statistical properties of images. An XGBoost model was trained on the features extracted by MRIQC on a
191 training subset of gold-standard images, and evaluated on a previously unseen test subset. The AUC was
192 also 0.99, matching the performance of our crowd-trained deep learning model.

193 **Braindr-based quality control has a substantial impact on effect size estimates**

194 The secondary goal of this study was to investigate how scaling expertise through citizen science amplification
195 affects scientific inferences from these data. For this proof of concept, we studied brain development, which is
196 the primary focus on the HBN dataset. Lebel and colleagues ([Lebel & Beaulieu, 2011](#)) found that increases
197 in white matter volume and decreases in gray matter volume are roughly equal in magnitude, resulting
198 in no overall brain volume change over development in late childhood. Based on Figure 2 in the Lebel
199 manuscript ([Lebel & Beaulieu, 2011](#)), we estimate an effect of approximately -4.3 cm^3 per year - a decrease
200 in gray matter volume over the ages measured (See Figure 2 in the the original manuscript; we estimate the
201 high point to be 710 cm^3 and the low point to be 580 cm^3 with a range of ages of approximately 5 years to
202 35 years and hence: $(710-580)/(5-35) = -4.3 \text{ cm}^3/\text{year}$). To reproduce their analysis and assess the effect of
203 using the CNN-derived quality control estimates, we estimated gray and white matter volume in the subjects
204 that had been scored for quality using our algorithm. Figure 4 shows gray matter volume as a function of age.
205 Two conditions are compared: in one (Figure 4A) all of the subjects are included, while in the other only
206 subjects that were passed by the CNN are included (Figure 4B, blue points). Depending on the threshold
207 chosen, the effect of gray matter volume over age varies from $-2.6 \text{ cm}^3/\text{year}$ (with no threshold) to -5.3
208 cm^3/year (with Braindr rating > 0.9). A threshold of 0.7 of either Braindr or MRIQC results in an effect
209 size around -4.3 cm^3 per year, replicating the results of ([Lebel & Beaulieu, 2011](#)). A supplemental interactive
210 version of this figure allows readers to threshold data points based on QC scores from the predicted labels
211 of the CNN (called “Braindr ratings”), or on MRIQC XGBoost probabilities (called “MRIQC ratings”) is
212 available at <http://results.braindr.us>. Thus, quality control has a substantial impact on estimates of

213 brain development and allowing poor quality data into the statistical model can almost entirely obscure
214 developmental changes in gray matter volume.

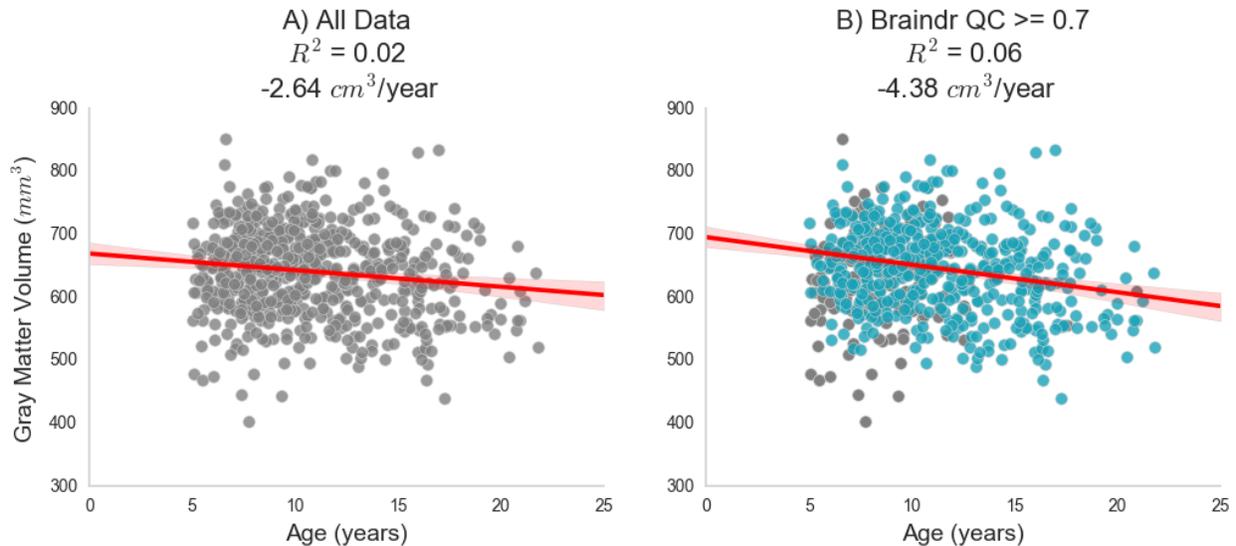


Figure 4: **Impact of quality control on effect size estimates:** Results of quality control on the inferred association between gray matter volume and age during development. Part A shows the relationship when all data is used in the ordinary least squares (OLS) model. Part B shows the new OLS model when data is thresholded by the deep learning model’s predicted braindr rating at 0.7. The effect size nearly doubles when QC scores are taken into account. See results.braindr.us for an interactive version of this figure.

215 Discussion

216 We have developed a system to scale expertise in neuroimaging to meet the demands of Big Data. The
217 system uses citizen scientists to amplify an initially-small, expert-labeled dataset. Combined with deep
218 learning (via CNNs), the system can then accurately perform image analysis tasks that require expertise,
219 such as quality control (QC). We have validated our method against MRIQC, a specialized tool that was
220 designed specifically for this use case based on knowledge of the physics underlying the signal generation
221 process in T1-weighted images (Esteban et al., 2017). Unlike MRIQC, our method is able to generalize
222 beyond quality control of T1-weighted images; any image-based binary classification task can be loaded onto
223 the Braindr platform, and crowdsourced via the web. For this use-case, we demonstrated the importance of
224 scaling QC expertise by showing how replication of a previously established results depends on a researcher’s
225 decision on data quality. Lebel and colleagues (Lebel & Beaulieu, 2011) report changes in gray matter

226 volume over development and we find that we only replicate these findings when using a stringent quality
227 control threshold for the input data.

228 **The Internet and Web Applications for Collaboration**

229 The internet and web browser technologies are not only crucial for scientific communication, but also for
230 collaboration and distribution of work. This is particularly true in the age of large consortium efforts aimed at
231 generating high-quality large data sets. Recent progress in citizen science projects for neuroscience research
232 have proven extremely useful and popular, in part due to the ubiquity of the web browser. Large-scale
233 citizen science projects, like EyeWire ([Kim et al., 2014](#); [Marx, 2013](#)), and Mozak ([Roskams & Popović,](#)
234 [2016](#)), have enabled scientists working with high resolution microscopy data to map neuronal connections
235 at the microscale, with help from over 100,000 citizen scientists. In MR imaging, web-based tools such
236 as BrainBox ([Heuer, Ghosh, Sterling, & Toro, 2016](#)) and Mindcontrol ([Keshavan et al., 2017](#)) were built to
237 facilitate the collaboration of neuroimaging experts in image segmentation and quality control. However,
238 the task of inspecting each slice of a 3D image in either BrainBox or Mindcontrol takes a long time, and this
239 complex task tends to lose potential citizen scientists who find it too difficult or time consuming. In general,
240 crowdsourcing is most effective when a project is broken down into short, simple, well-defined “micro-tasks”,
241 that can be completed in short bursts of work and are resilient to interruption ([Cheng, Teevan, Iqbal, &](#)
242 [Bernstein, 2015](#)). In order to simplify the task for citizen scientists, we developed a web application called
243 braindr, which reduces the time-consuming task of slice-by-slice 3D inspection to a quick binary choice made
244 on a 2D slice. While we might worry that distilling a complex decision into a simple swipe on a smartphone
245 might add noise, we demonstrated that a model could be constructed to accurately combine ratings from
246 many citizen scientists to almost perfectly emulate those obtained from inspection by experts. Using braindr,
247 citizen scientists amplified the initial expert-labelled dataset (200 3D images) to the entire dataset (> 700
248 3D images, > 3000 2D slices) in a few weeks. Because braindr is a lightweight web application, users could
249 play it at any time and on any device, and this meant we were able to attract many users. On braindr,
250 each slice received on average 20 ratings, and therefore each 3D brain (consisting of 5 slices) received on
251 average 100 ratings. In short, by redesigning the way we interact with our data and presenting it in the web
252 browser, we were able to get many more eyes on our data than would have been possible in a single research
253 lab.

254 **Scaling expertise through interactions between experts, citizen scientists and** 255 **machine learning**

256 We found that an interaction between experts, citizen scientists, and machine learning results in scalable
257 decision-making on brain MRI images. Recent advances in machine learning have vastly improved image
258 classification(Krizhevsky, Sutskever, & Hinton, 2012), object detection(Girshick, Donahue, Darrell, & Malik,
259 2014), and segmentation(Long, Shelhamer, & Darrell, 2015) through the use of deep convolutional neural net-
260 works. In the biomedical domain, these networks have been trained to accurately diagnose eye disease (Lee,
261 Baughman, & Lee, 2017), diagnose skin cancer (Esteva et al., 2017), and breast cancer (Sahiner et al., 1996),
262 to name a few applications. But these applications require a large and accurately labeled dataset. This
263 presents an impediment for many scientific disciplines, where labeled data may be more scarce, or hard to
264 come by, because it requires labor-intensive procedures. The approach presented here solves this fundamen-
265 tal bottleneck in the current application of modern machine learning approaches, and enables scientists to
266 automate complex tasks that require substantial expertise.

267 A surprising finding that emerges from this work is that a deep learning algorithm can learn to match or
268 even exceed the aggregated ratings that are used for training. This finding is likely to reflect the fact that
269 algorithms are more reliable than humans, and when an algorithm is trained to match human accuracy, it has
270 the added benefit of perfect reliability. For example even an expert might not provide the exact same ratings
271 each time they see the same image, while an algorithm will. This is in line with findings from (Lee, Tying,
272 et al., 2017a), showing that the agreement between an algorithm and any one expert can be equivalent to
273 agreement between any pair of experts. We have demonstrated that while an individual citizen scientist
274 may not provide reliable results, by intelligently combining a crowd with machine learning, and keeping an
275 expert in the loop to monitor results, decisions can be accurately scaled to meet the demands of Big Data.

276 **MRI Quality Control and Morphometrics over Development**

277 The specific use-case that we focused on pertains to the importance of quality control in large-scale MRI
278 data acquisitions. Recently, Ducharme and colleagues (Ducharme et al., 2016b) stressed the importance of
279 quality control for studies of brain development in a large cohort of 954 subjects. They estimated cortical

280 thickness on each point of a cortical surface and fit linear, quadratic and cubic models of thickness versus
281 age at each vertex. Quality control was performed by visual inspection of the reconstructed cortical surface,
282 and removing data that failed QC from the analysis. Without stringent quality control, the best fit models
283 were more complex (quadratic/cubic), and with quality control the best fit models were linear. They found
284 sex differences only at the occipital regions, which thinned faster in males. In the supplemental figure that
285 accompanies Figure 4, we presented an interactive chart where users can similarly explore different ordinary
286 least squares models (linear or quadratic) and also split by sex for the relationship between total gray matter
287 volume, white matter volume, CSF volume, and total brain volume over age.

288 We chose to QC raw MRI data in this study, rather than the processed data because the quality of the
289 raw MRI data affects the downstream cortical mesh generation, and many other computed metrics. A
290 large body of research in automated QC of T1-weighted images exists, in part because of large open data
291 sharing initiatives. In 2009, Mortamet and colleagues ([Mortamet et al., 2009](#)) developed a QC algorithm
292 based on the background of magnitude images of the Alzheimer’s Disease Neuroimaging Initiative (ADNI)
293 dataset, and reported a sensitivity and specificity of $> 85\%$. In 2015, Shehzad and colleagues ([Shehzad et al., 2015](#))
294 developed the Preprocessed Connectomes Project Quality Assessment Protocol (PCP-QAP) on
295 the Autism Brain Imaging Data Exchange (ABIDE) and Consortium for Reproducibility and Reliability
296 (CoRR) datasets. The PCP-QAP also included a Python library to easily compute metrics such as signal
297 to noise ratio, contrast to noise ratio, entropy focus criterion, foreground-to-background energy ratio, voxel
298 smoothness, and percentage of artifact voxels. Building on this work, the MRIQC package from Esteban
299 and colleagues ([Esteban et al., 2017](#)) includes a comprehensive set of 64 image quality metrics, from which a
300 classifier was trained to predict data quality of the ABIDE dataset for new, unseen sites with 76% accuracy.

301 Our strategy differed from that of the MRIQC classification study. In the Esteban 2017 study ([Esteban et al.,](#)
302 [2017](#)), the authors labelled images that were “doubtful” in quality as a “pass” when training and evaluating
303 their classifier. Our MRIQC classifier was trained and evaluated only on images that our raters very confi-
304 dently passed or failed. Because quality control is subjective, we felt that it was acceptable for a “doubtful”
305 image to be failed by the classifier. Since our classifier was trained on data acquired within a single site, and
306 only on images that we were confident about, our MRIQC classifier achieved near perfect accuracy with an
307 AUC of 0.99. On the other hand, our braindr CNN was trained as a regression (rather than a classification)

308 on the full dataset, including the “doubtful” images (i.e those with ratings closer to 0.5), but was still eval-
309 uated as a classifier against data we were confident about. This also achieved near-perfect accuracy with
310 an AUC of 0.99. Because both the MRIQC and braindr classifiers perform so well on data we are confident
311 about, we contend that it is acceptable to let the classifier act as a “tie-breaker” for images that lie in the
312 middle of the spectrum, for future acquisitions of the HBN dataset.

313 Quality control of large consortium datasets, and more generally, the scaling of expertise in neuroimaging,
314 will become increasingly important as neuroscience moves towards data-driven discovery. Interdisciplinary
315 collaboration between domain experts and computer scientists, and public outreach and engagement of
316 citizen scientists can help realize the full potential of Big Data.

317 **Limitations**

318 One limitation of this method is that there is an interpretability-to-speed tradeoff. Specialized QC tools
319 were developed over many years, while this study was performed in a fraction of that time. Specialized QC
320 tools are far more interpretable; for example, the coefficient of joint variation (CJV) metric from MRIQC
321 is sensitive to the presence of head motion. CJV was one of the most important features of our MRIQC
322 classifier, implying that our citizen scientists were primarily sensitive to motion artifacts. This conclusion is
323 difficult to come to when interpreting the braindr CNN. Because we employed transfer learning, the features
324 that were extracted were based on the ImageNet classification task, and it is unclear how these features
325 related to MRI-specific artifacts. However, interpretability of deep learning is an ongoing active field of
326 research ([Chakraborty et al., 2017](#)), and we may be able to fit more interpretable models in the future.

327 Compared to previous efforts to train models to predict quality ratings, such as MRIQC ([Esteban et al.,](#)
328 [2017](#)), our AUC scores are very high. There are two main reasons for this. First, in the Esteban 2017
329 study ([Esteban et al., 2017](#)), the authors tried to predict the quality of scans from unseen sites, whereas in
330 our study, we combined data across the two sites from which data had been made publicly available at the
331 time we conducted this study. Second, even though our quality ratings on the 3D dataset were continuous
332 scores (ranging from -5 to 5), we only evaluated the performance of our models on data that received an
333 extremely high (4,5) or extremely low score (-4,-5) by the experts. This was because quality control is very

334 subjective, and therefore, there is more variability on images that people are unsure about. An image that
335 was failed with low confidence (-3 to -1) by one researcher could conceivably be passed with low confidence
336 by another researcher (1 to 3). Most importantly, our study had enough data to exclude the images within
337 this range of relative ambiguity in order to train our XGBoost model on both the braindr ratings and the
338 MRIQC features. In studies with less data, such an approach might not be feasible.

339 Another limitation of this method was that our citizen scientists were primarily neuroscientists. The braindr
340 application was advertised on Twitter (<https://www.twitter.com>) by the authors, whose social networks
341 (on this platform) primarily consisted of neuroscientists. As the original tweet travelled outside our social
342 network, we saw more citizen scientists without experience looking at brain images on the platform, but the
343 number of ratings they contributed were not as high as those with neuroscience experience. We also saw that
344 there was an overall tendency for all our users to incorrectly pass images. Future iterations of braindr will
345 include a more informative tutorial and random checks with known images throughout the game to make
346 sure our players are well informed and are performing well throughout the task. In this study, we were able
347 to overcome this limitation because we had enough ratings to train the XGBoost algorithm to preferentially
348 weight some user's ratings over others.

349 **Future Directions**

350 Citizen science platforms like the Zooniverse ([Simpson, Page, & De Roure, 2014](#)) enable researchers to
351 upload tasks and engage over 1 million citizen scientists. We plan to integrate braindr into a citizen science
352 platform like Zooniverse. This would enable researchers to upload their own data to braindr, and give them
353 access to a diverse group of citizen scientists, rather than only neuroscientists within their social network.
354 We also plan to reuse the braindr interface for more complicated classification tasks in brain imaging. An
355 example could be the classification of ICA components as signal or noise ([Griffanti et al., 2017](#)), or the
356 evaluation of segmentation algorithms. Finally, incorporating braindr with existing open data initiatives,
357 like OpenNeuro ([K. Gorgolewski, Esteban, Schaefer, Wandell, & Poldrack, 2017](#)), or existing neuroimaging
358 platforms like LORIS ([Das, Zijdenbos, Vins, Harlap, & Evans, 2012](#)) would enable scientists to directly
359 launch braindr tasks from these platforms, which would seamlessly incorporate human in the loop data
360 analysis in neuroimaging research. More generally, the principles described here motivate platforms that

361 integrate citizen science with deep learning for Big Data applications across the sciences.

362 **Methods**

363 **The Healthy Brain Network Dataset**

364 The first two releases of the Healthy Brain Network dataset were downloaded from <http://fcon.1000>
365 [.projects.nitrc.org/indi/cmi_healthy_brain_network/sharing_neuro.html](http://projects.nitrc.org/indi/cmi_healthy_brain_network/sharing_neuro.html) . A web application for
366 brain quality control, called Mindcontrol (Keshavan et al., 2017) was hosted at <https://mindcontrol-hbn>
367 [.herokuapp.com](http://herokuapp.com) , which enabled users to view and rate 3D MRI images in the browser. There were 724 T1-
368 weighted images. All procedures were approved by the University of Washington Institutional Review Board
369 (IRB). Mindcontrol raters, who were all neuroimaging researchers with substantial experience in similar
370 tasks, provided informed consent, including consent to publicly release these ratings. Mindcontrol raters
371 were asked to pass or fail images after inspecting the full 3D volume, and provide a score of their confidence
372 on a 5 point Likert scale, where 1 was the least confident and 5 was the most confident. Mindcontrol raters
373 received a point for each new volume they rated, and a leaderboard on the homepage displayed rater rankings.
374 The ratings of the top 4 expert raters (including the lead author) were used to create a gold-standard subset
375 of the data.

376 **Gold-standard Selection**

377 The gold-standard subset of the data was created by selecting images that were confidently passed or con-
378 fidently failed (confidence equal or larger than 4) by the 4 expert raters. In order to measure reliability
379 between expert raters, the ratings of the second, third, and fourth expert expert rater were recoded to a
380 scale of -5 to 5 (where -5 is confidently failed, and 5 is confidently passed). An ROC analysis was performed
381 against the binary ratings of the lead author on the commonly rated images, and the area under the curve
382 (AUC) was computed for each pair. An average AUC, weighted by the number of commonly rated images
383 between the pair, was 0.97, showing good agreement between expert raters. The resulting gold-standard
384 dataset consisted of 200 images. Figure 5 shows example axial slices from the gold-standard dataset. The

385 gold-standard dataset set contains 100 images that were failed by experts, and 100 images that were passed
by experts.

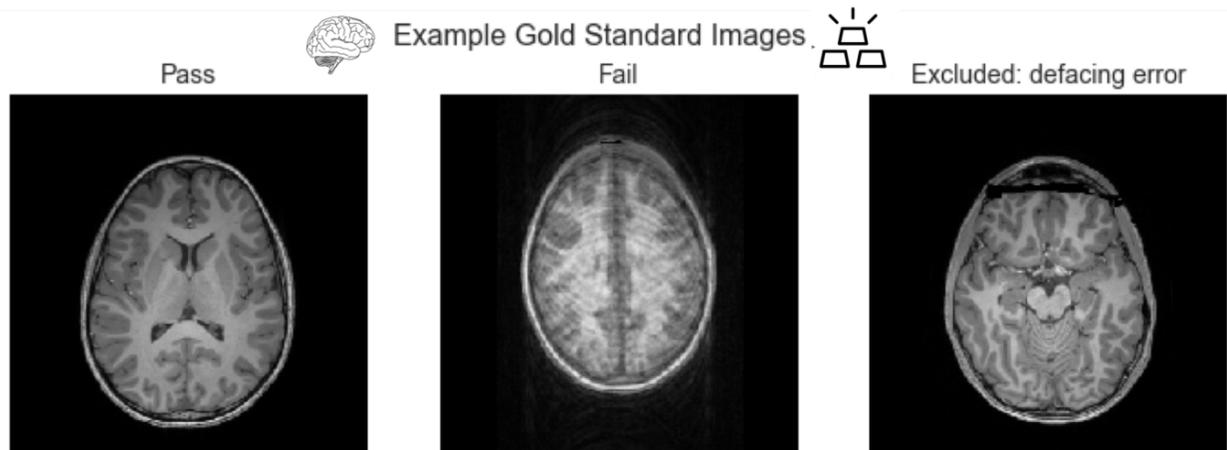


Figure 5: **Example axial slices from the gold-standard dataset:** Passed images show clear contrast between tissue types, and failed images primarily consisted of those with large motion artifacts. We excluded images that failed because of defacing errors from this analysis.

386

387 Data Preparation

388 All images were then converted into a set of 2D axial slices using the NiBabel Python library (Brett et al.,
389 2018) and uploaded to <https://braindr.us>. Two images of the 724 were corrupted, so the total image
390 count became 722 images. Five slices, separated by 40 slices, were selected from each brain, where the first
391 slice was one that had over 10,000 non-zero pixels. All slices were padded to 256x256 or 512x512 depending
392 on original image size. One subject (sub-NDARVJ504DAA) had only 4 slices because the last slice did not
393 meet the 10,000 pixel threshold. The total number of slices uploaded to <https://braindr.us> was 3609.

394 The braindr web application

395 The braindr application was written in Javascript using the Vue.js (<https://vuejs.org>) framework. Google
396 Firebase (<https://firebase.google.com/>) was used for the realtime database. The axial brain slices were
397 hosted on Amazon S3 and served over the Amazon CloudFront content delivery network. Figure 6 shows the
398 braindr interface, which presents to the user a 2D slice. On a touchscreen device (tablet or mobile phone),
399 users can swipe right to pass or swipe left to fail the image. On a desktop, a user may click the “pass” or

400 “fail” button or use the right or left arrow keys to classify the image. The user receives a point for each
401 rating, unless they rate against the majority, where the majority is defined only for images with more than 5
402 ratings, and where the average rating is below 0.3 or above 0.7. The user receives a notification of the point
403 they earned (or did not earn) for each image after each swipe. All users electronically signed a consent form
404 as approved by the University of Washington IRB. Images were initially served randomly, and then images
405 with fewer ratings were preferentially served.

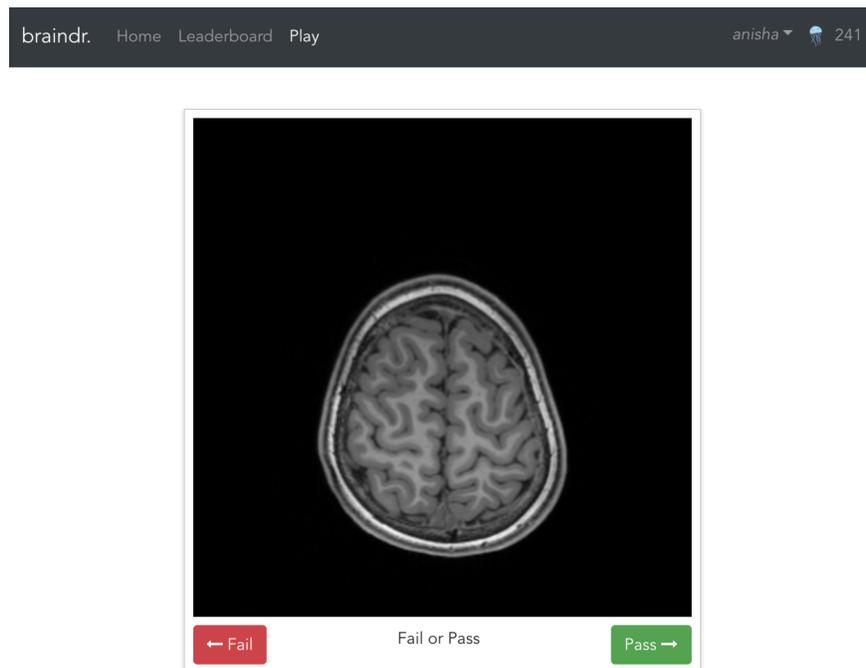


Figure 6: **The braindr web interface:** Braindr was hosted at <https://braindr.us>. Users may click pass or fail buttons, use arrow keys, or swipe on a touchscreen device to rate the image. The top right shows the user’s score.

406

407 **Braindr data collection**

408 A total of 261 users submitted over 80,000 ratings. We selected the 25% of the users who rated the largest
409 numbers of the gold-standard slices. This reduced the dataset to 65 users who submitted 68,314 total ratings,
410 18,940 of which were on the 1000 gold-standard slices. Figure 7 shows the distribution of average ratings
411 and the distribution of number of ratings per slice on the gold-standard dataset.

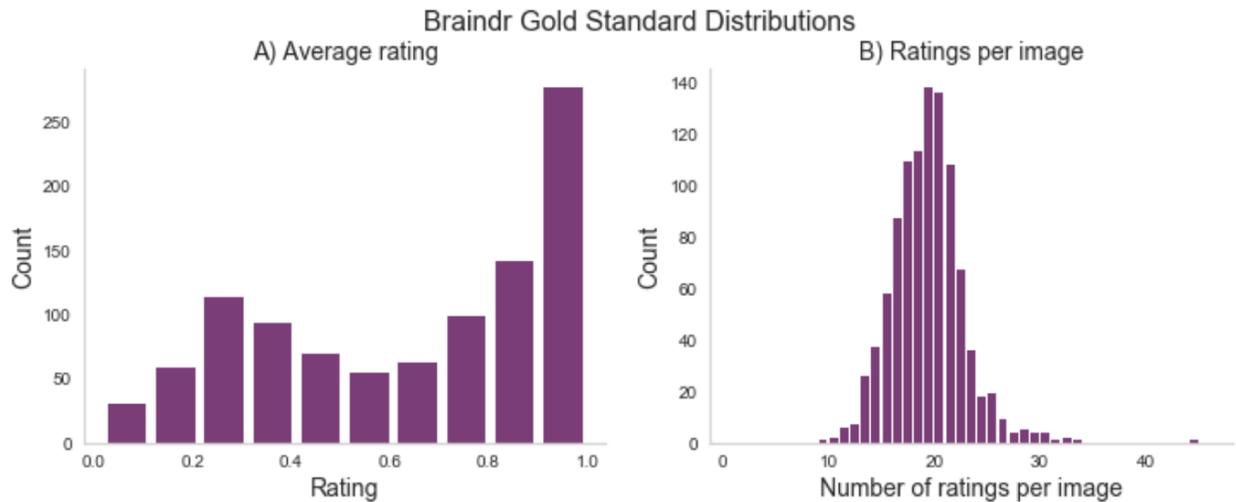


Figure 7: **BrainDR data distributions:** Part A shows the distribution of average ratings for each slice on the gold-standard slices. Part B shows the number of ratings per slice, where on average each slice received 20 ratings.

412 Rating aggregation with XGBoost

413 To aggregate citizen scientist ratings, we weighted citizen scientists based on how consistent their rat-
414 ings were with the gold-standard. We trained an XGBoost classifier (Chen & Guestrin, 2016b) imple-
415 mented in Python (http://xgboost.readthedocs.io/en/latest/python/python_intro.html) using the
416 cross-validation functions from the scikit-learn Python library (Pedregosa et al., 2011). We used 600 es-
417 timators, and grid searched over a stratified 10-fold cross-validation within the training set to select the
418 optimal maximum depth (2 vs 6) and learning rate (0.01, 0.1). The features of the model were the citizen
419 scientists and each observation was a slice, with the entries in the design matrix set to be the average rating
420 of a specific citizen scientist on a particular slice. We trained the classifier on splits of various sizes of the
421 data to test the dependence on training size (see Figure 2A). We used the model trained with $n=670$ to
422 extract the probability scores of the classifier on all 3609 slices in braindr (see Figure 2B). While equally
423 weighting each citizen scientist’s ratings results in a bimodal distribution with a lower peak that is shifted
424 up from zero (Figure 7A), the distribution of probability scores in Figure 2B more accurately matches our
425 expectations of the data; a bimodal distribution with peaks at 0 and 1. Feature importances were extracted
426 from the model and plotted in Figure 2C, and plotted against total number of gold-standard image ratings
427 in Figure 2D.

428 **Deep learning to predict image QC label**

429 Finally, a deep learning model was trained on the brain slices to predict the XGBoost probability score. All
430 brain slices were resized to 256 by 256 pixels and converted to 3 color channels (RGB) to be compatible with
431 the VGG16 input layer. The data was split into 80%-10%-10% training-validation-test sets. The data was
432 split such that all slices belonging to the same subject were grouped together, so that any individual subject
433 could be only in either training, validation or test. We loaded the VGG16 network that was pretrained with
434 ImageNet weights (Simonyan & Zisserman, 2014) implemented in Keras (Chollet et al., 2015), removed
435 the top layer, and ran inference on all the data. The output of the VGG16 inference was then used to
436 train a small sequential neural network consisting of a dense layer with 256 nodes and a rectified linear unit
437 activation function (ReLU), followed by a dropout layer set to drop 50% of the weights to prevent overfitting,
438 and finally a single node output layer with sigmoid activation. The training of the final layer was run for
439 50 epochs and the best model on the validation set across the 50 epochs was saved. We ran this model 10
440 separate times, each time with a different random initialization seed, in order to measure the variability of
441 our ROC AUC on the test set.

442 **Training the MRIQC model**

443 MRIQC was run on all images in the HBN dataset. Rather than using the previously trained MRIQC
444 classifier from Esteban and colleagues (Esteban et al., 2017), the extracted QC features were used to train
445 another XGBoost classifier to predict gold-standard labels. Two thirds of the data was used to train the
446 model, where a 2-fold cross-validation was used to optimize hyper parameters: learning rate = 0.001, 0.01,
447 0.1, number of estimators = 200, 600, and maximum depth = 2,6,8. An ROC analysis was run, and the
448 computed area under the curve was 0.99.

449 **Gray matter volume vs age during development**

450 Finally, to explore the relationship between gray matter volume and age over development as a function
451 of QC threshold, gray matter volume was computed from running the Mindboggle software (Klein et al.,
452 2017) on the entire dataset. Mindboggle combines the image segmentation output from Freesurfer (Fischl,
453 2012) with that of ANTS (Avants et al., 2011) to improve the accuracy of segmentation, labeling and volume

454 shape features. Extremely low quality scans did not make it through the entire Mindboggle pipeline, and as
455 a result the dataset size was reduced to 629 for this part of the analysis. The final QC score for the brain
456 volumes was computed by taking the average of the predicted braindr rating from the deep learning model
457 for all five slices. We ran an ordinary least squares (OLS) model on gray matter volume versus age on the
458 data with and without QC thresholding, where the QC threshold was set at 0.7. Figure 4 shows the result
459 of this analysis, which showed an effect size that nearly doubled and replicated previous findings when QC
460 was performed on the data.

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475 Code and Data Availability

476 The code for the braindr application can be found at <https://doi.org/10.5281/zenodo.1208140>. The
477 brain slice data and model weights are hosted at <https://osf.io/j5d4y/> . The code for the analysis
478 for this project, including all figures and the source code for the interactive version of this manuscript,

479 can be found at <https://github.com/akeshavan/braindr-results> (including the Jupyter notebook for
480 the full analysis at [https://github.com/akeshavan/braindr-results/blob/master/notebooks/braindr
-full-v0.3.ipynb](https://github.com/akeshavan/braindr-results/blob/master/notebooks/braindr-
481 -full-v0.3.ipynb)) and <https://github.com/akeshavan/braindr-analysis> (which also has the origi-
482 nal Mindcontrol quality ratings at [https://raw.githubusercontent.com/akeshavan/braindr-analysis/
master/braindrAnalysis/data/mindcontrol-feb-21-18_anon.json](https://raw.githubusercontent.com/akeshavan/braindr-analysis/
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